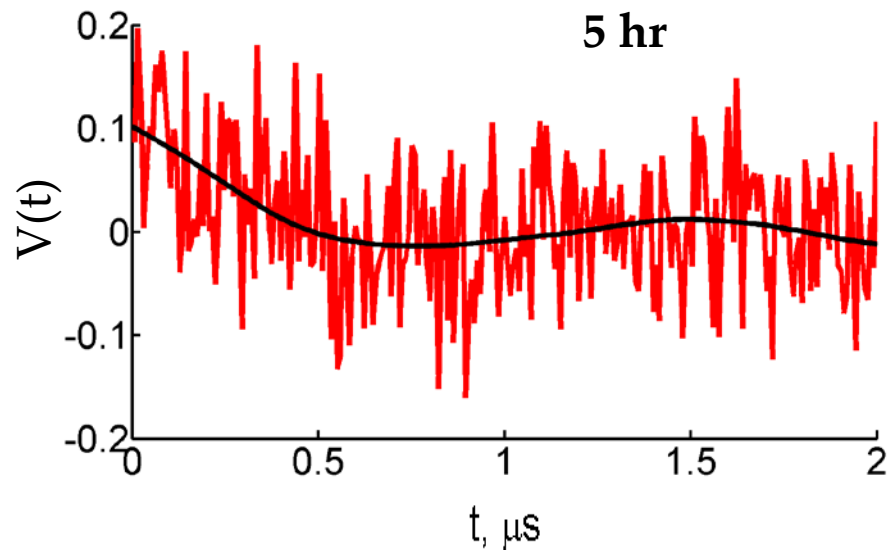
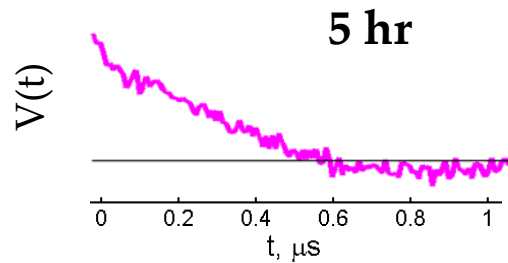


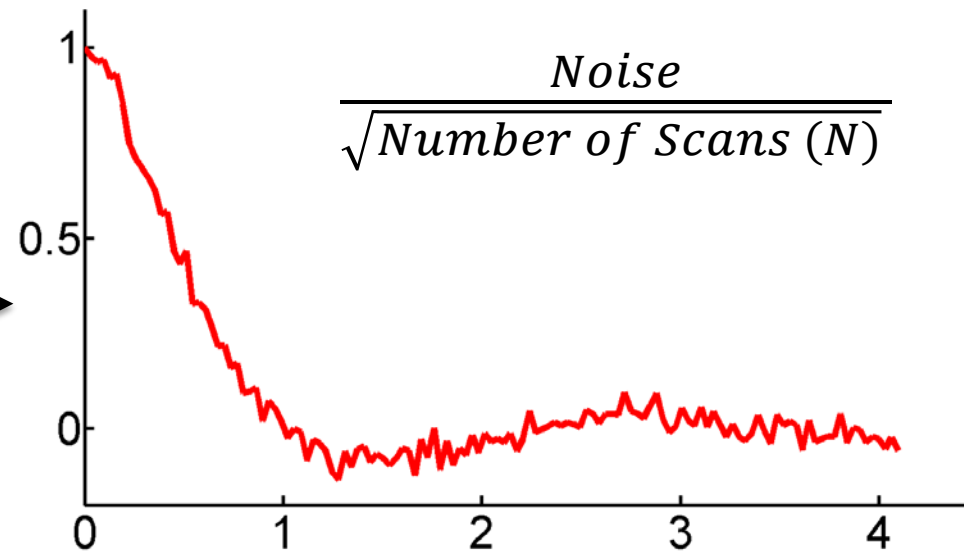
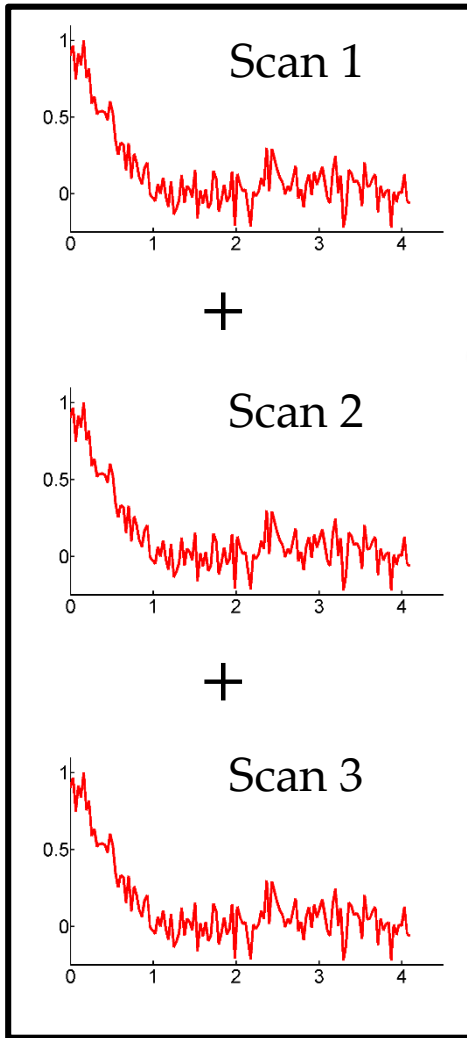
Principles of Wavelet Denoising for ESR

- Jack Freed
- Madhur Srivastava

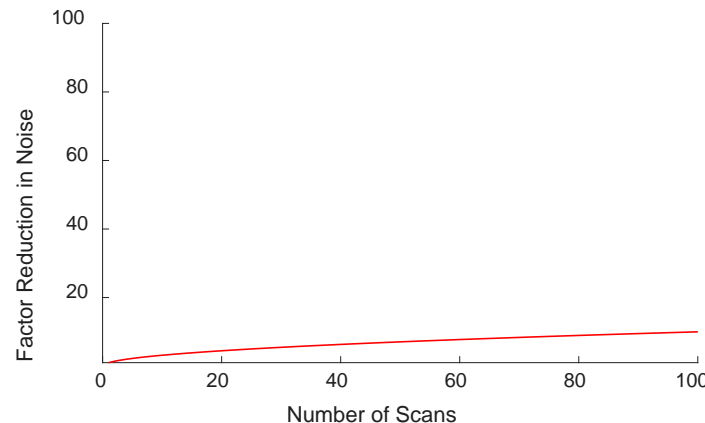


17 GHz DQC data for two anion radicals from flavin cofactors of a membrane receptor. Phase-memory time is $\sim 1 \mu\text{s}$ and radical yield is relatively low.

The DQC signal (in black), buried under overwhelming noise, was extracted by de-noising and its first half coincides with a better signal (magenta) obtained using a half of the sampling period.

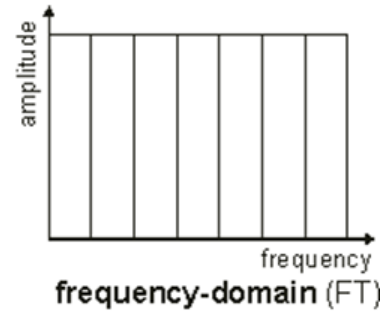
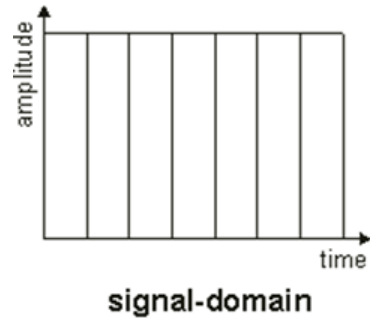


Noise Reduction Rate in Signal Averaging



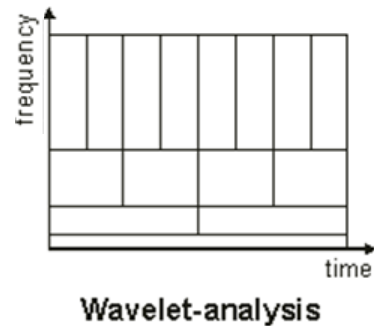
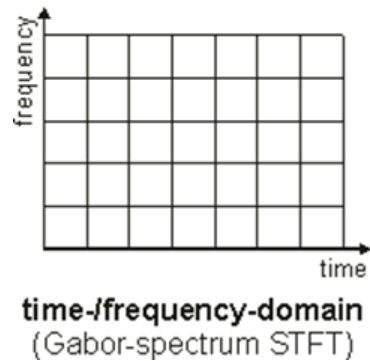
Disadvantages:

- Long Acquisition Times
- Sample Breakdown
- High Sample Concentration Needed
- Instrument Drifts and Malfunction
- Inability to Acquire Signals from Unstable Samples



FT

$$F(\omega) = \int_{-\infty}^{+\infty} f(t)e^{-i\omega t} dt$$



STFT

$$F(\tau, \omega) = \int_{-\infty}^{+\infty} f(t)w(t - \tau)e^{-i\omega t} dt$$

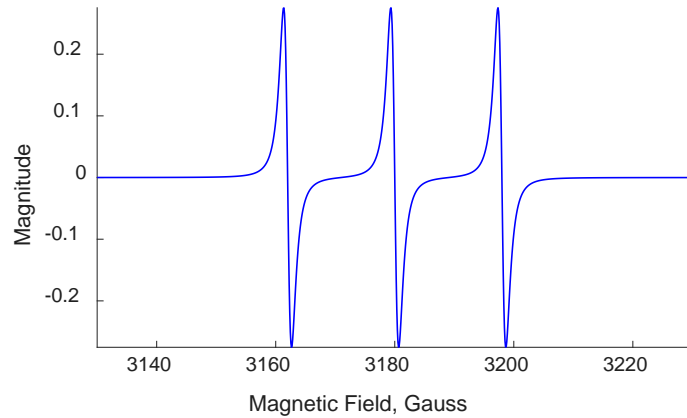
WT

$$F(a, b) = \frac{1}{\sqrt{a}} \int_{-\infty}^{+\infty} f(t) \psi^* \left(\frac{t - b}{a} \right) dt$$

Inverse Frequency

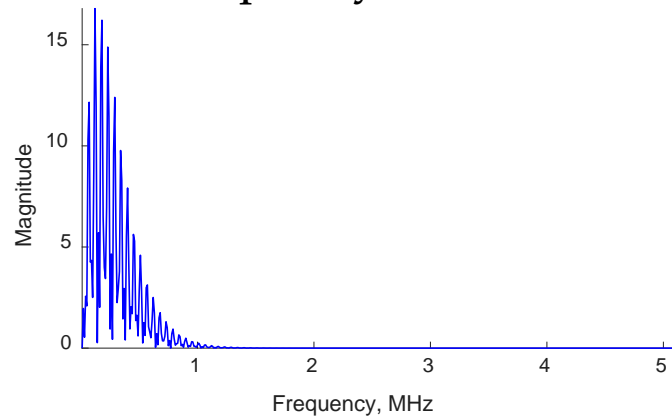
Time Displacement

a cw-ESR Spectra

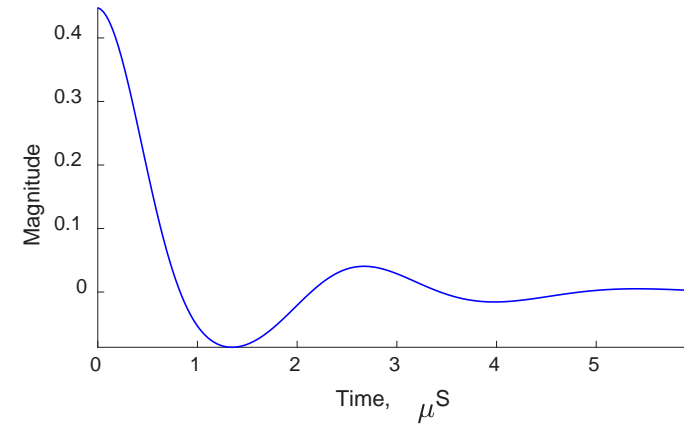


↓ **Fourier Transform**

b Frequency Information

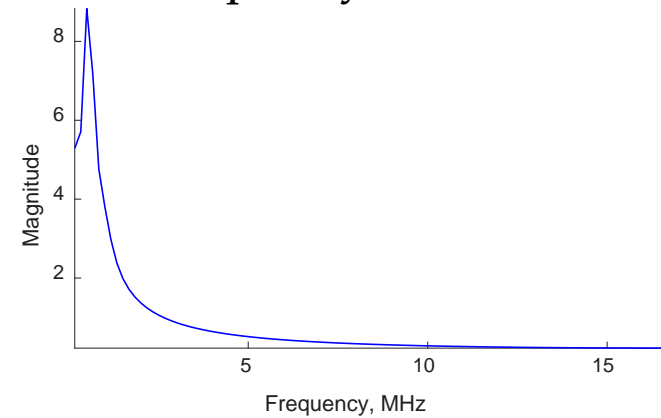


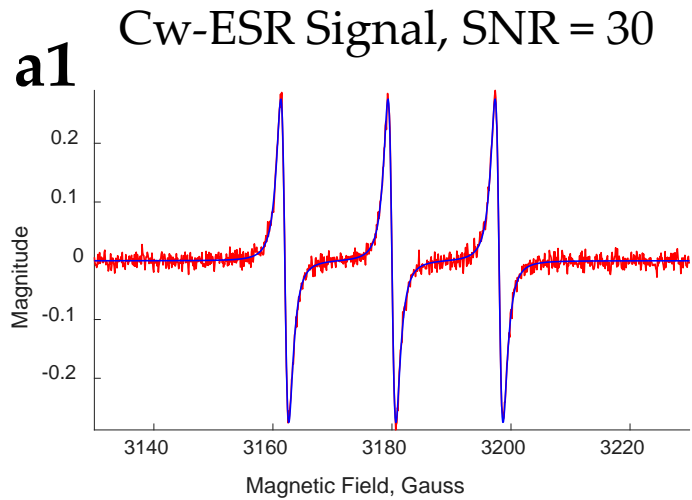
a Pulsed Dipolar Signal



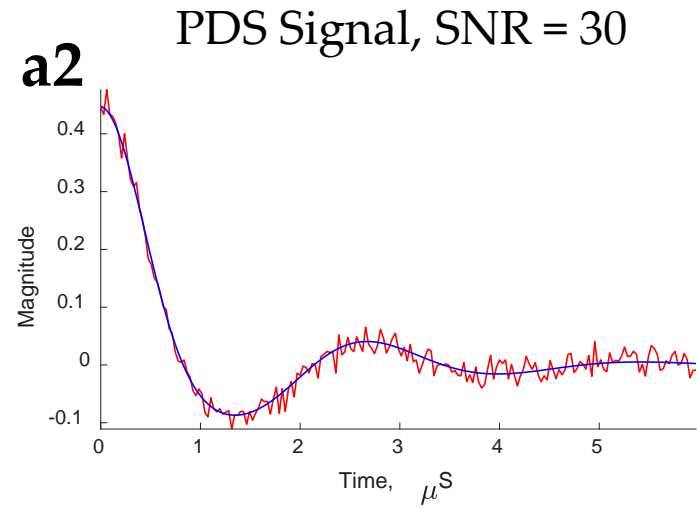
↓ **Fourier Transform**

b Frequency Information





- Noise-free
- Noisy

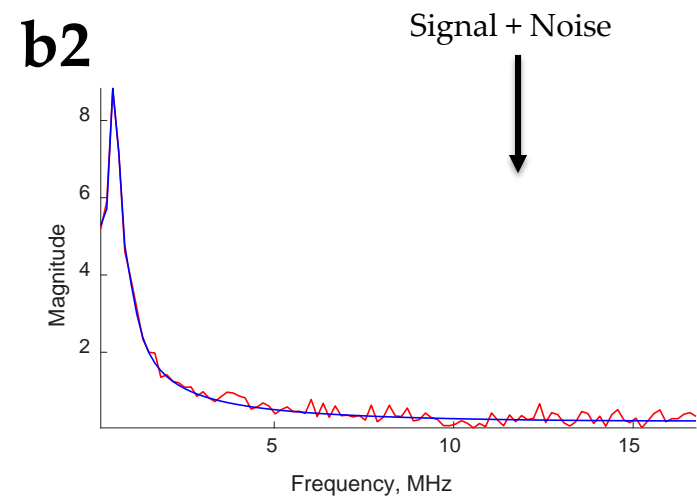
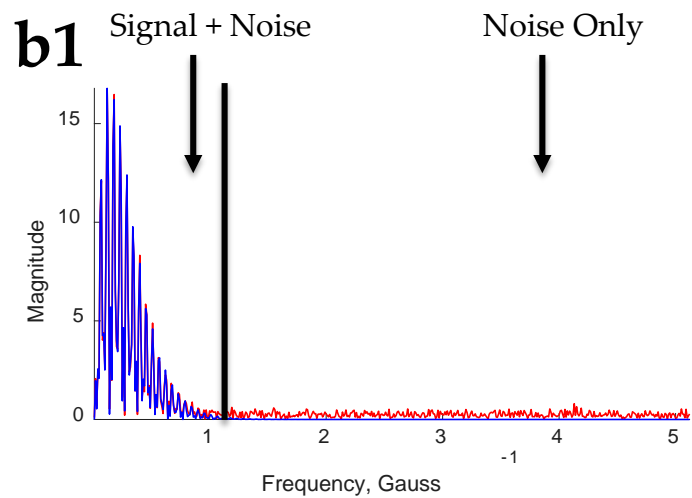


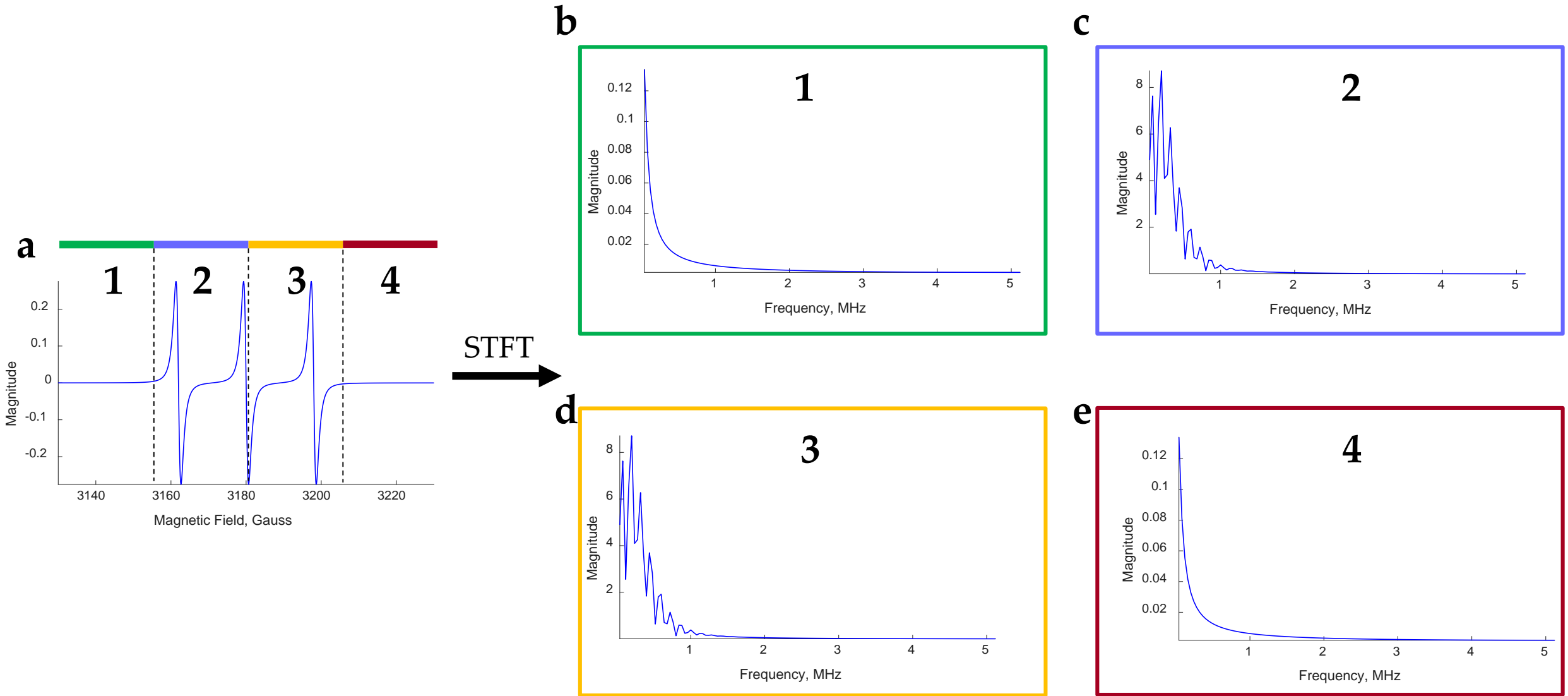
Disadvantages: Limits Fourier Filtering

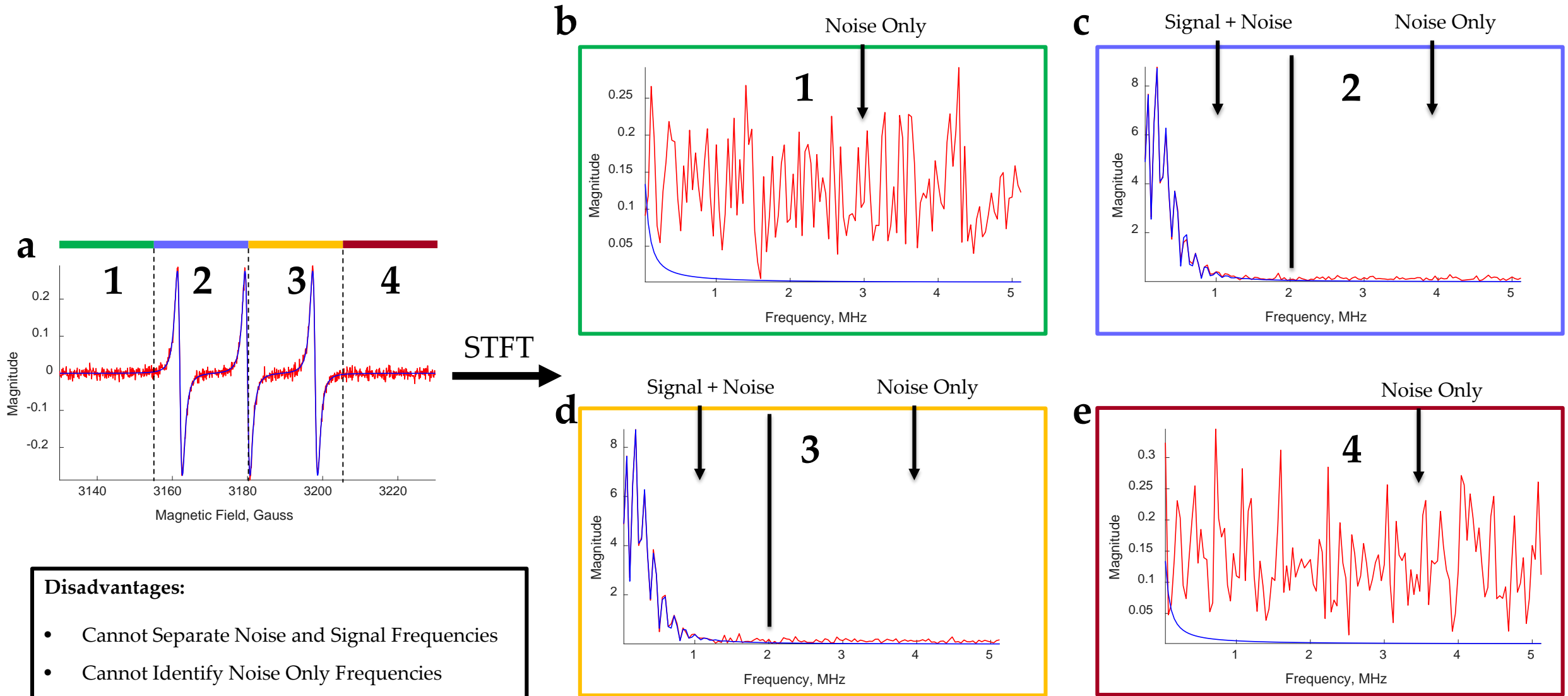
- Cannot Separate Noise and Signal Frequencies
- Cannot Identify Noise Only Frequencies

Fourier Transform

Fourier Transform

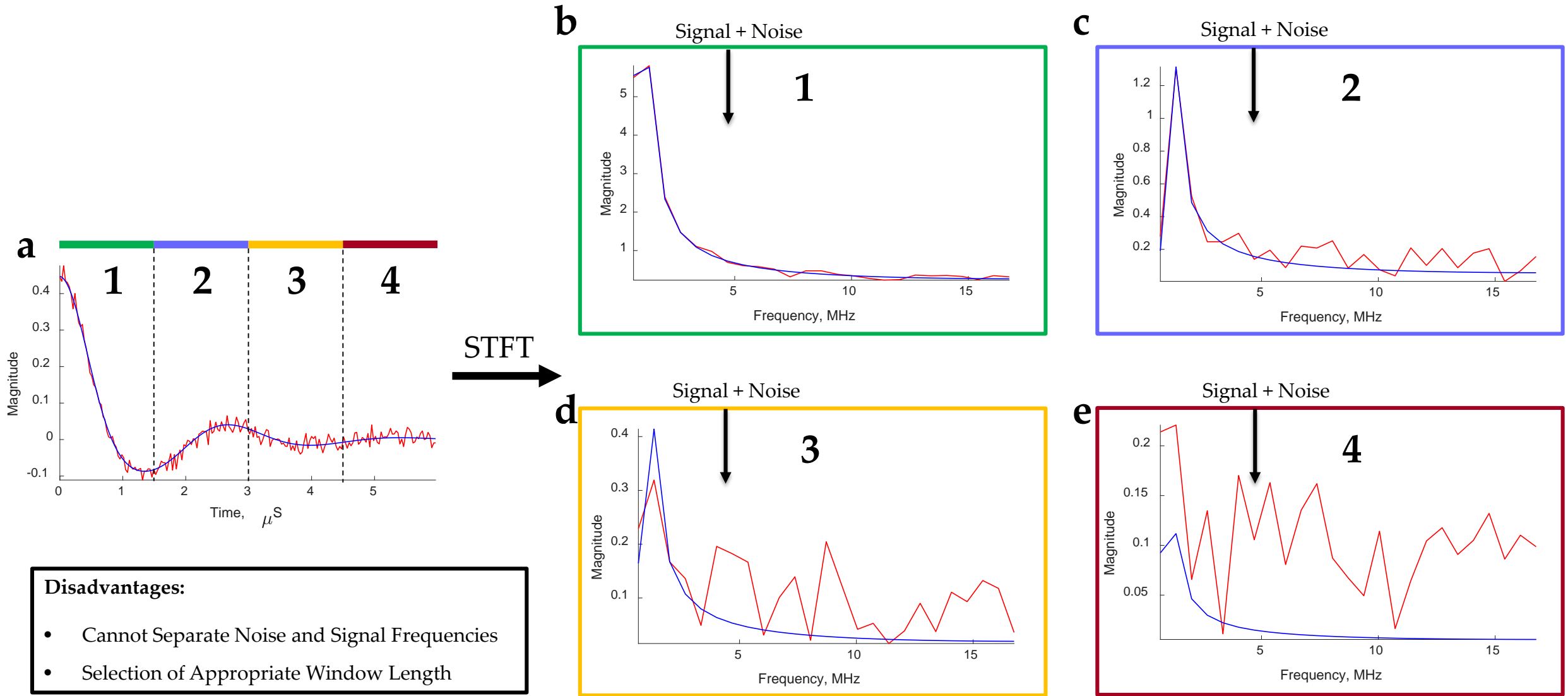






Disadvantages:

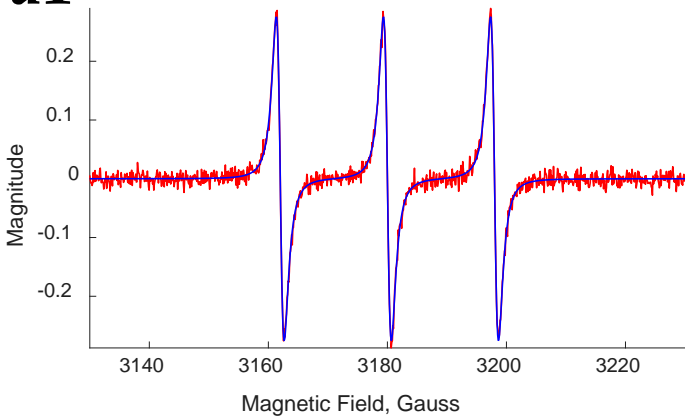
- Cannot Separate Noise and Signal Frequencies
- Cannot Identify Noise Only Frequencies
- Selection of Appropriate Window Length



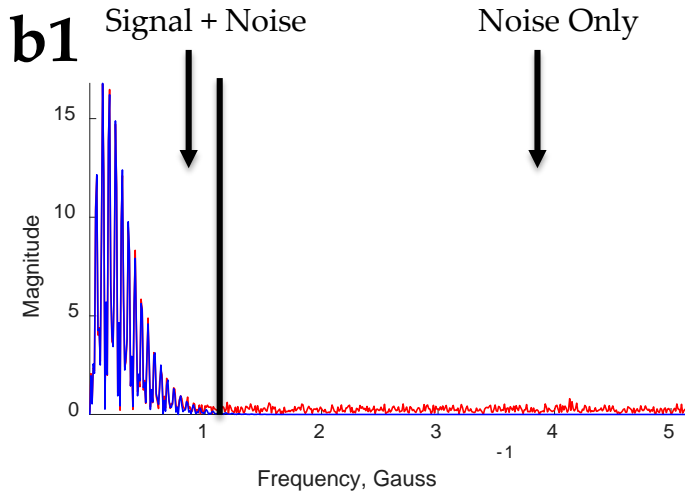
Disadvantages:

- Cannot Separate Noise and Signal Frequencies
- Selection of Appropriate Window Length

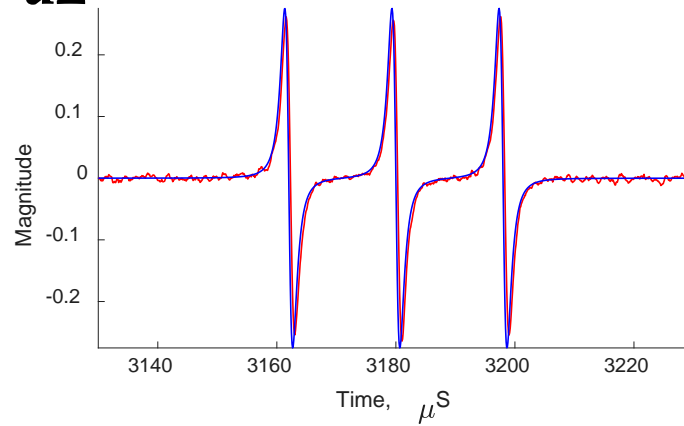
a1 Cw-ESR Signal, SNR = 30



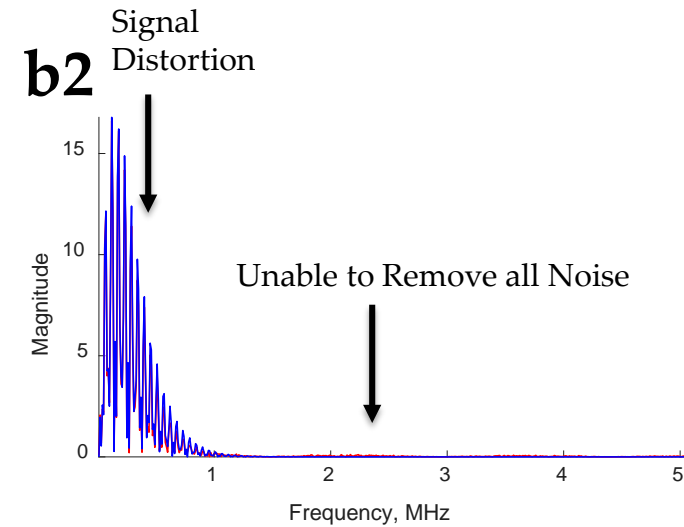
Fourier Transform



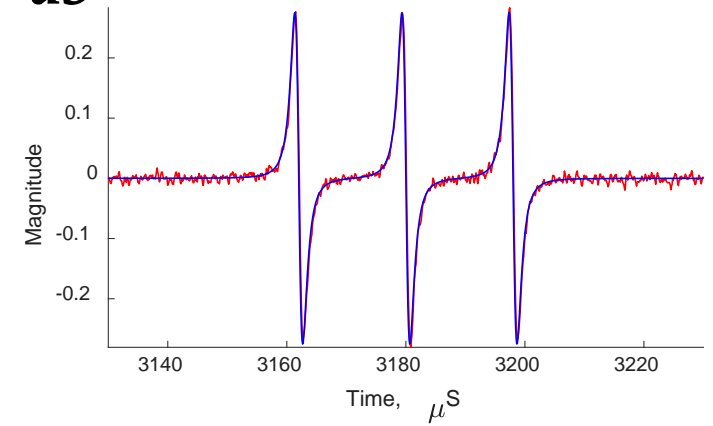
a2 Low Pass Filtering



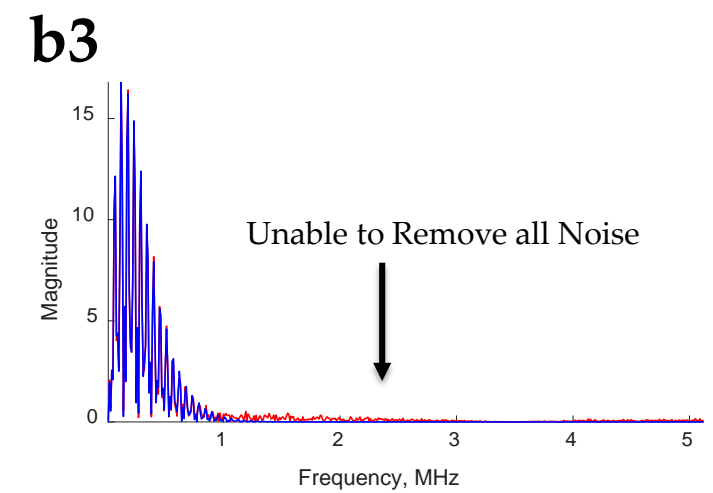
Fourier Transform

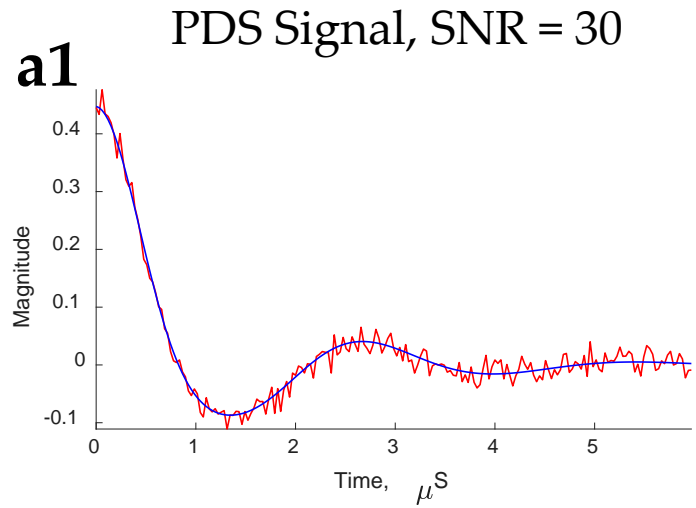


a3 Gaussian Filtering

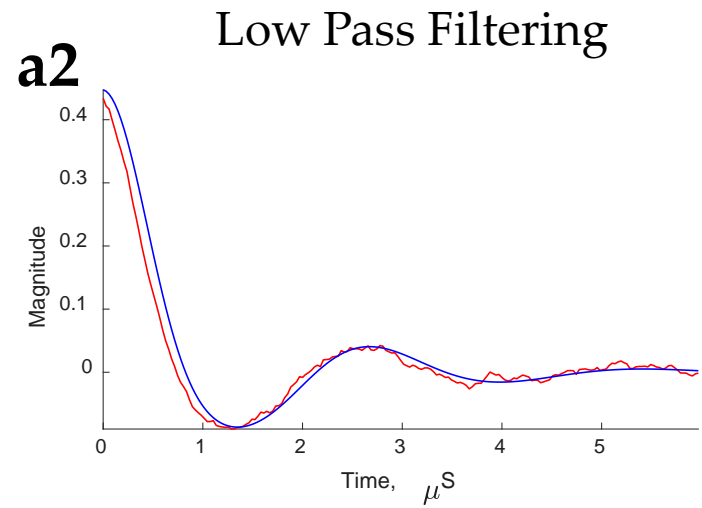
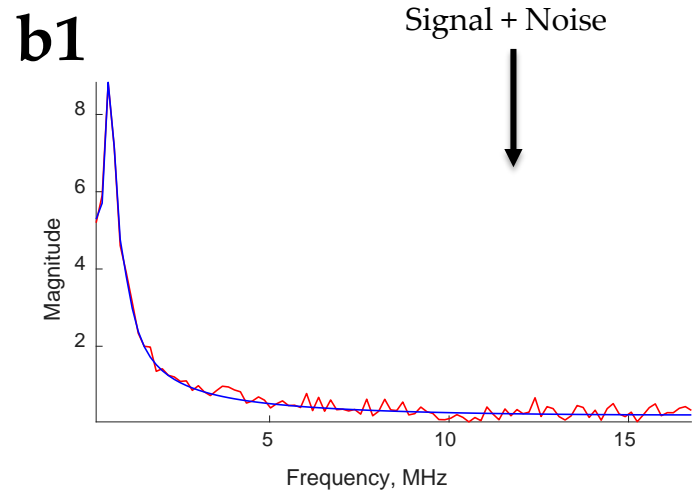


Fourier Transform

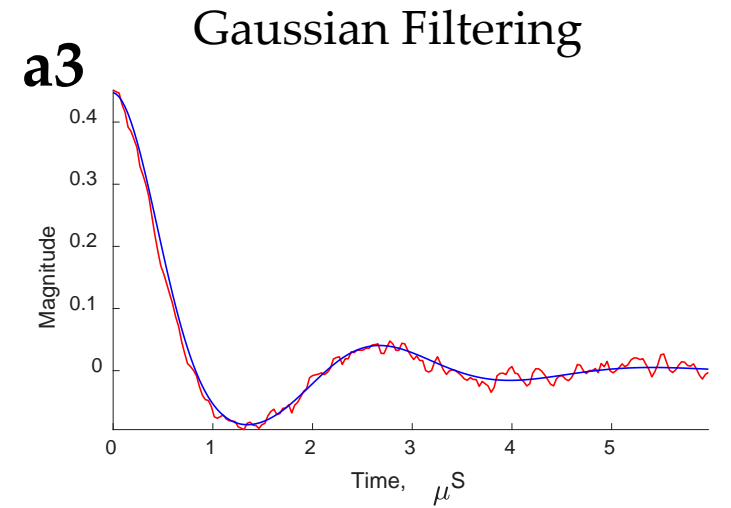
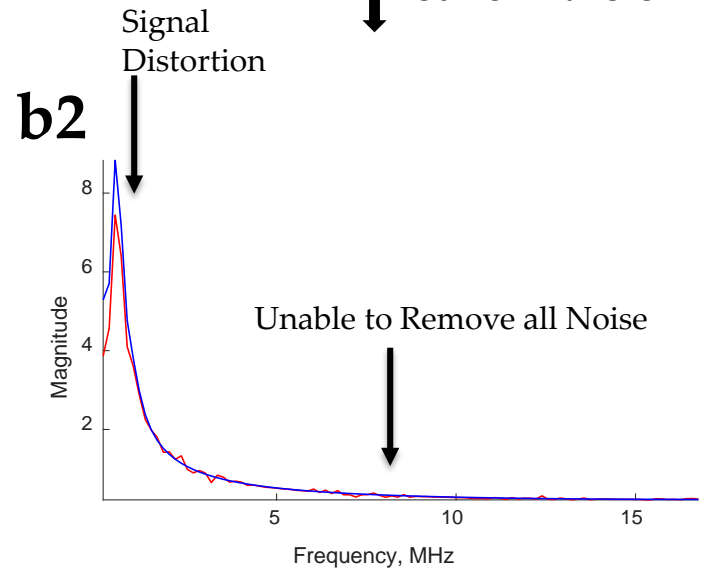




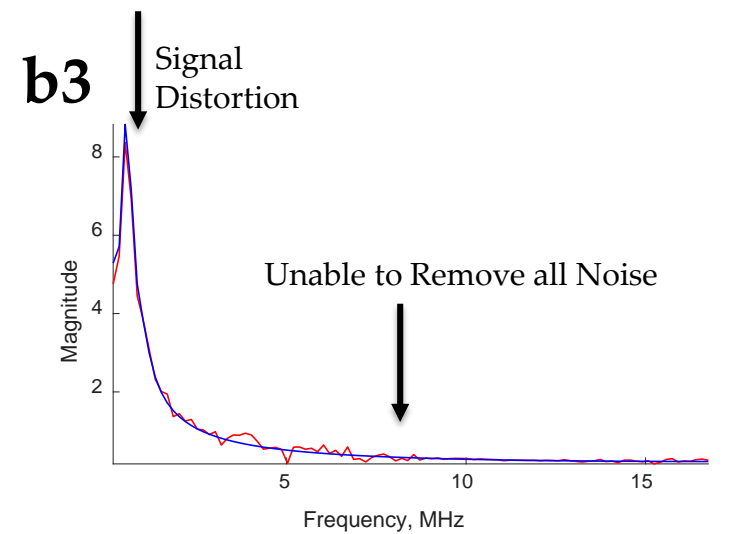
Fourier Transform



Fourier Transform



Fourier Transform



Need a method that can provide signal and its frequency information simultaneously

Continuous Wavelet Transform (CWT)

$$F(a, b) = \frac{1}{\sqrt{a}} \int_{-\infty}^{+\infty} f(t) \psi^* \left(\frac{t - b}{a} \right) dt$$

Discrete Wavelet Transform (DWT)

$$D[a, b] = \frac{1}{\sqrt{a}} \sum_{m=1}^p f[t_m] \psi \left(\frac{t_m - b}{a} \right)$$

Logarithmic Discretization

$$D_j[k] = \frac{1}{\sqrt{a_0^j}} \sum_{m=1}^p f[t_m] \psi \left(\frac{t_m - kb_0 a_0^j}{a_0^j} \right)$$

Dyadic Discretization

$$D_j[k] = \frac{1}{\sqrt{2^j}} \sum_{m=1}^p f[t_m] \psi \left(\frac{t_m - k2^j}{2^j} \right)$$

D = Detail or Wavelet Component

j = Decomposition level: positive integers

k = Translation parameter: positive integers

t_m = Discrete signal at integer time or location m

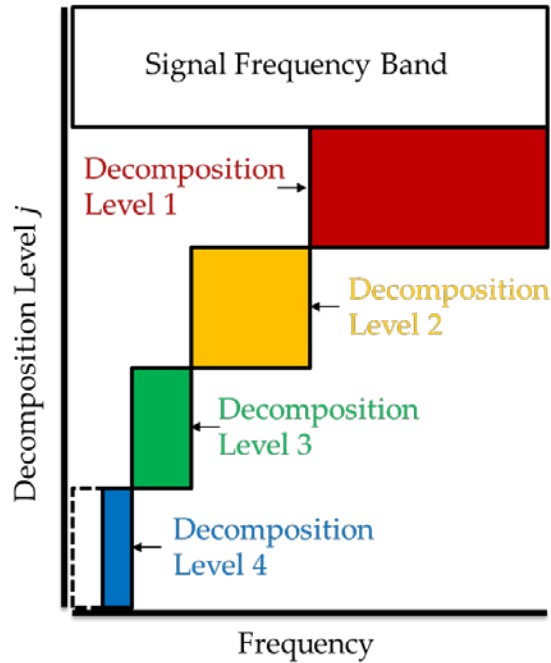
p = Length of discrete input signal $f[t_m]$

ϕ = Scaling function

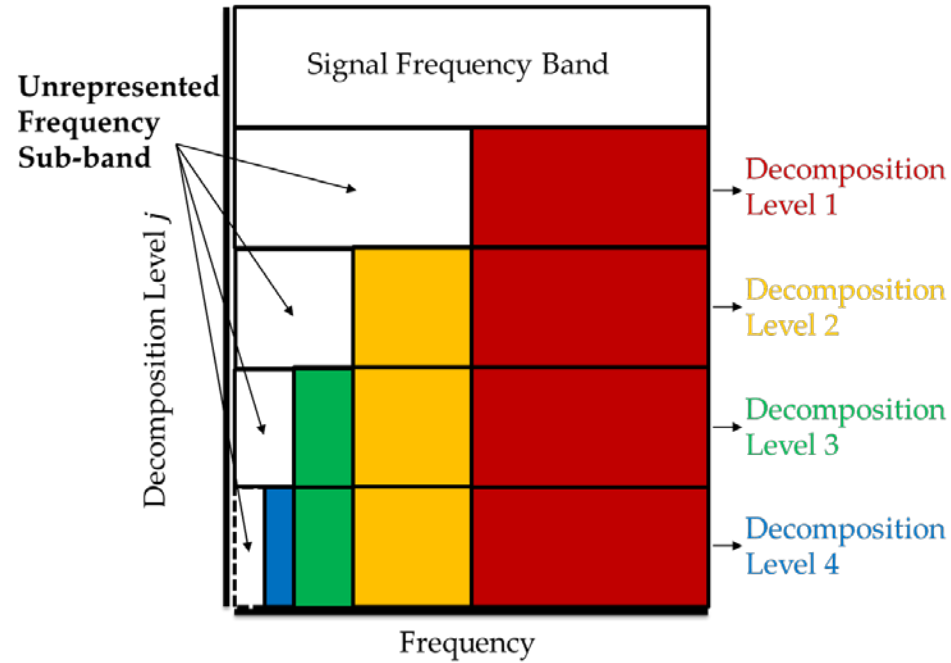
ψ = Wavelet function

Dyadic Discretization: $b = k2^j$
 $a = 2^j$

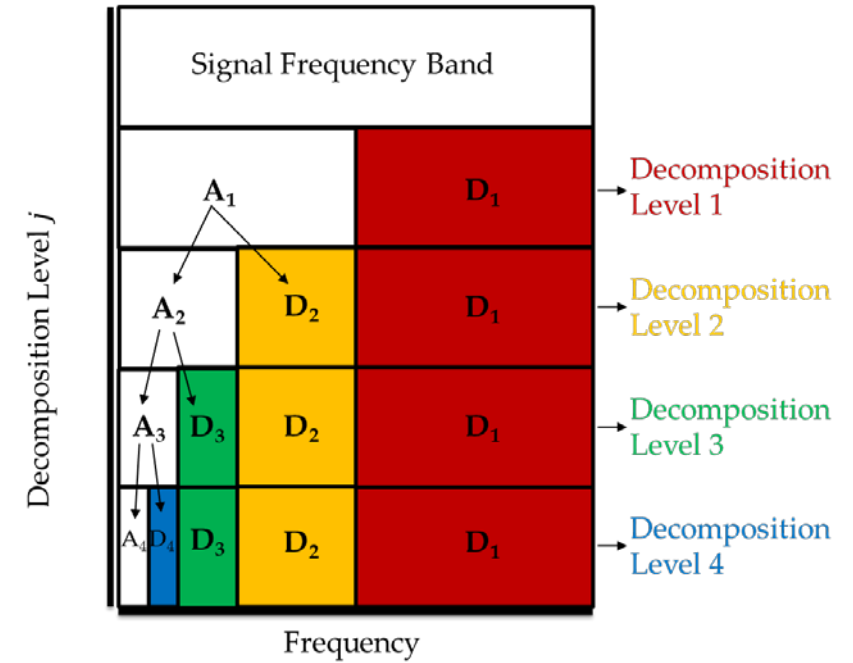
Frequency Sub-band Division in Wavelet Domain



Frequency Sub-band Representation at Each Decomposition Level



Detail and Approximation Component Representation



Scaling Function

$$\phi(t_m) = (-1)^k c_k \psi(2t_m - k)$$

Approximation Component

$$A_j[k] = \frac{1}{\sqrt{2^j}} \sum_{m=1}^p f[t_m] \phi\left(\frac{t_m - k2^j}{2^j}\right)$$

A = Approximation or Residual Component

j = Decomposition level: positive integers

k = Translation parameter: positive integers

t_m = Discrete signal at integer time or location m

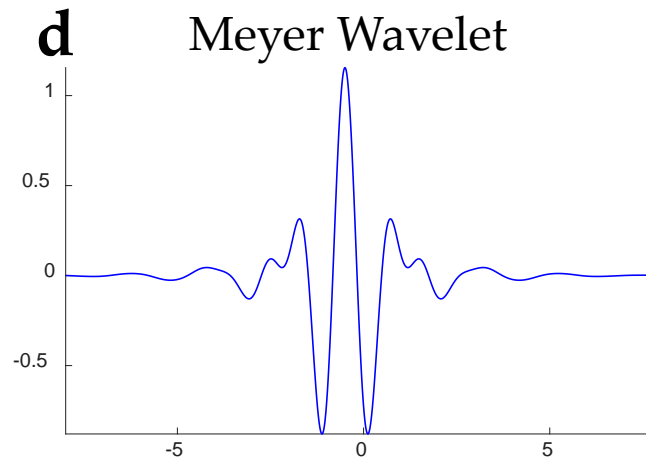
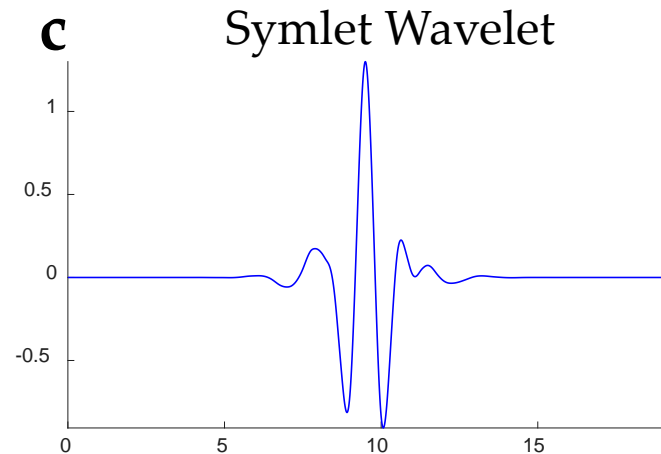
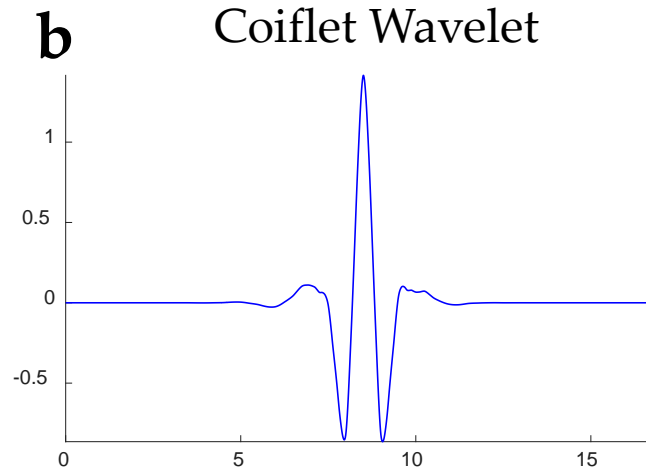
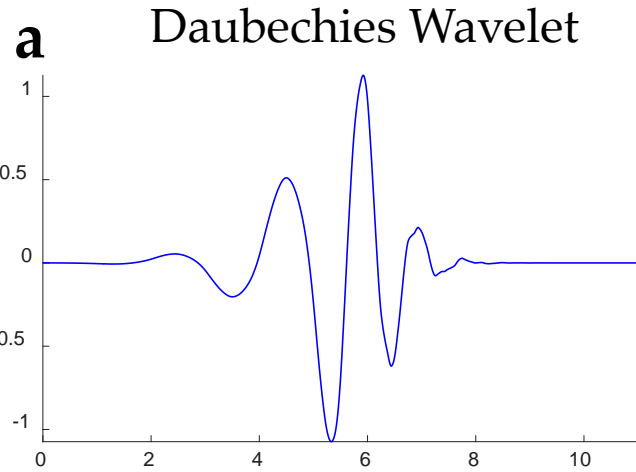
p = Length of discrete input signal $f[t_m]$

ϕ = Scaling function

ψ = Wavelet function

c_k = Coefficients of wavelet function

Dyadic Discretization: $b = k2^j$
 $a = 2^j$

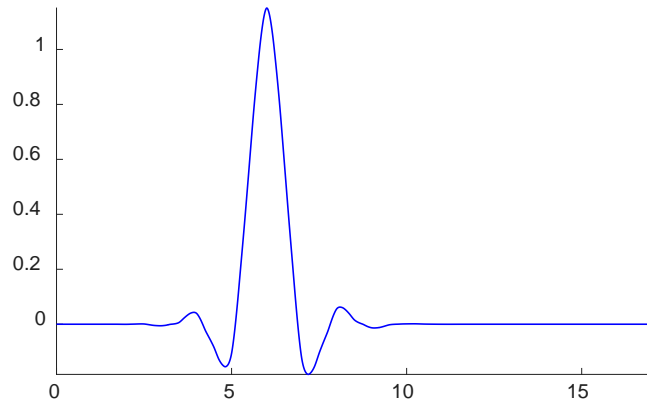


Low Computational Complexity

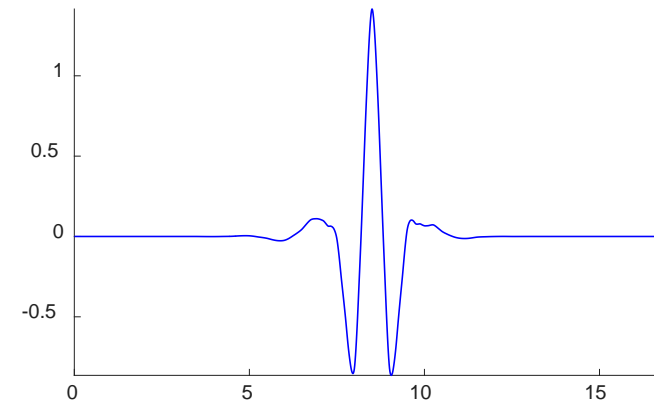
$O(p)$, where p is discrete signal length. 10ms for data length 4096 on a 64-bit operating system with 16 GB RAM and a 3.30 GHz processor

FFT: $O(p \log p)$

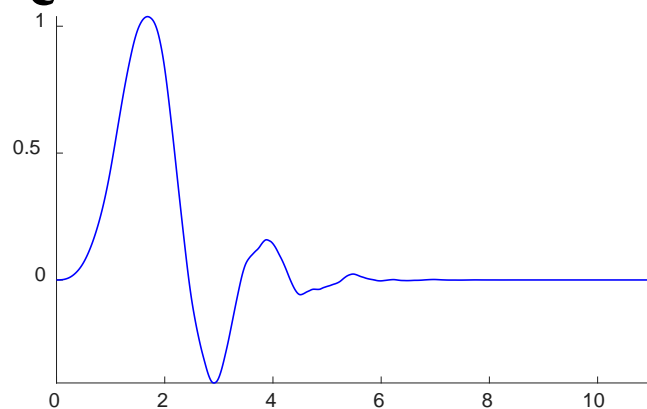
a Coif-3: Scaling Function



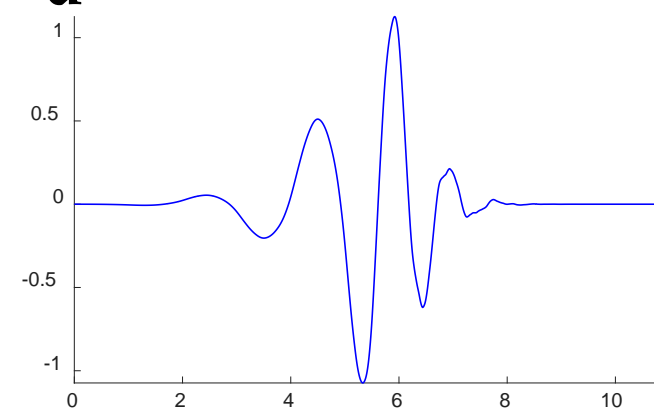
b Coif-3: Wavelet Function

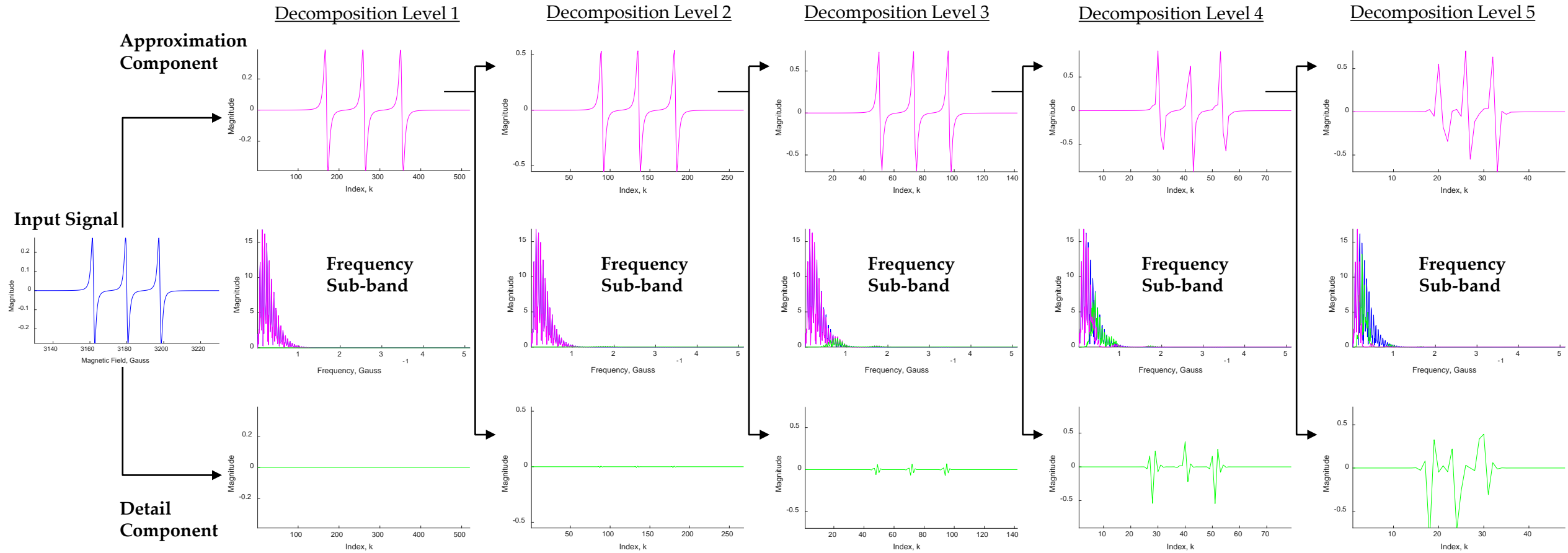


c db-6: Scaling Function



d db-6: Wavelet Function





Signal Displacement (Field Sweep)

$$F(a, b) = \frac{1}{\sqrt{a}} \int_{-\infty}^{+\infty} f(t) \psi^* \left(\frac{t-b}{a} \right) dt$$

Inverse Frequency

Detail Component is always centered around 0 because it represents non-zero frequency, i.e. relative change

Inverse Discrete Wavelet Transform (IDWT)

$$f[t_m] = \sum_{k=1}^{p_j} A_{j_0}[k] \phi\left(\frac{t_m - k2^{j_0}}{2^N}\right) + \sum_{j=1}^{j_0} \sum_{k=1}^{p_j} D_j[k] \psi\left(\frac{t_m - k2^j}{2^j}\right)$$

Orthonormality of the DWT

$$\sum_{t=1}^L \psi\left(\frac{t_m - k2^j}{2^j}\right) \phi\left(\frac{t_m - k'2^{j'}}{2^{j'}}\right) = 0, \quad \forall j \leq j'$$

$$\sum_{t=1}^L \psi\left(\frac{t_m - k2^j}{2^j}\right) \psi\left(\frac{t_m - k'2^{j'}}{2^{j'}}\right) = \begin{cases} 1, & \text{if } j = j' \text{ and } k = k' \\ 0, & \text{otherwise} \end{cases}$$

Relationship Between Wavelet and Scaling Function

$$|\Phi(\omega)|^2 = \sum_{j=j'+1}^{\infty} \frac{|\Psi(2^{-j}\omega)|^2}{2^{-j}}$$

p_j = Length of the j^{th} Detail/
Approximation
component.

L = Discrete length
of the wavelet and
scaling functions.

N = Maximum
number of
decomposition
levels, $\lfloor \log_2 p \rfloor$

j_0 = Arbitrary
decomposition level
where $1 \leq j_0 \leq N$

Decomposition Level 5

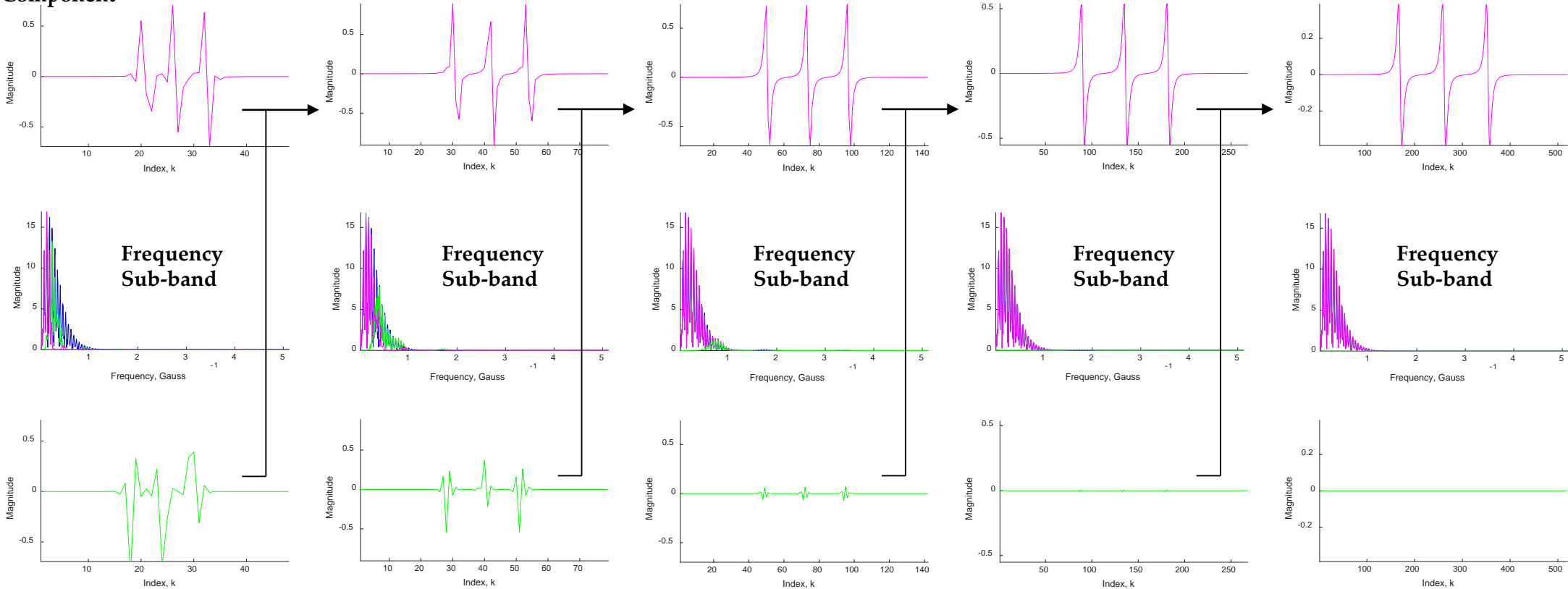
Decomposition Level 4

Decomposition Level 3

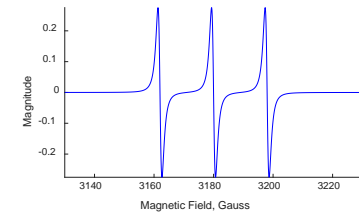
Decomposition Level 2

Decomposition Level 1

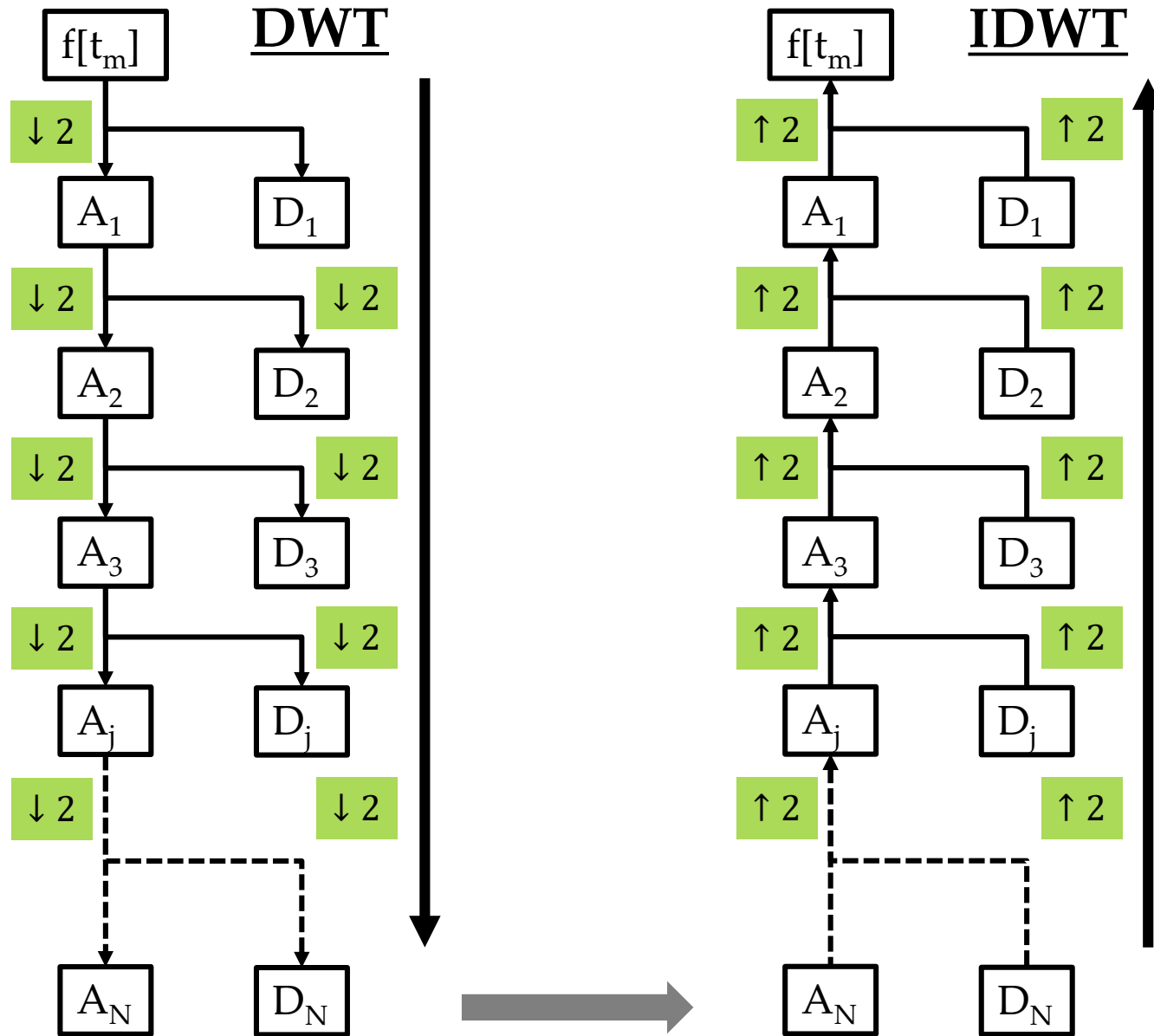
Approximation Component

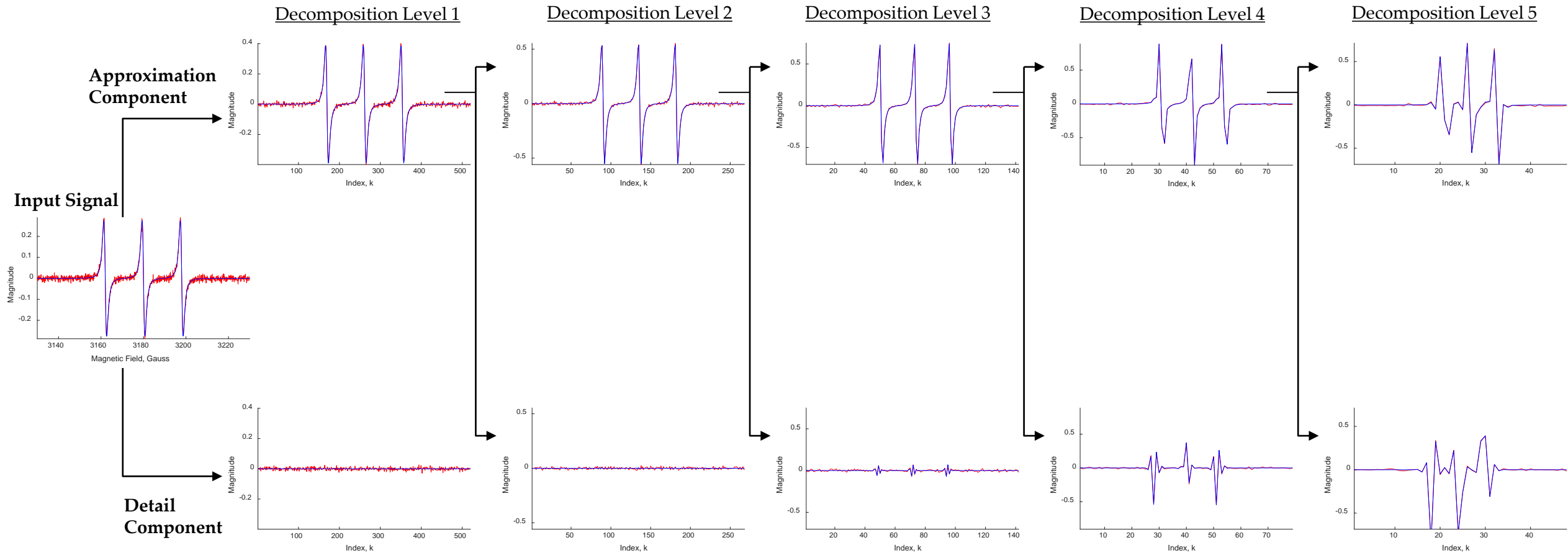


Input Signal



Detail Component

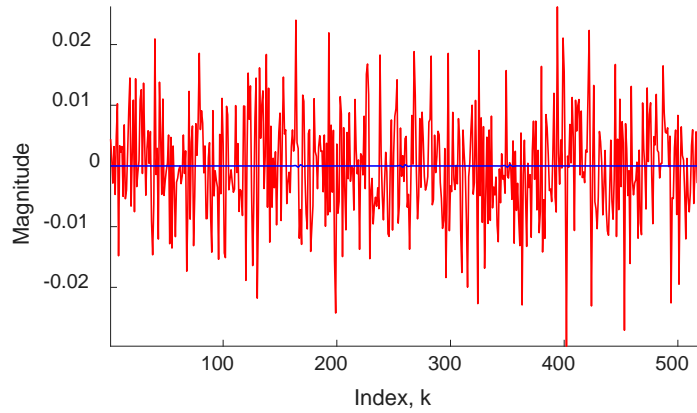




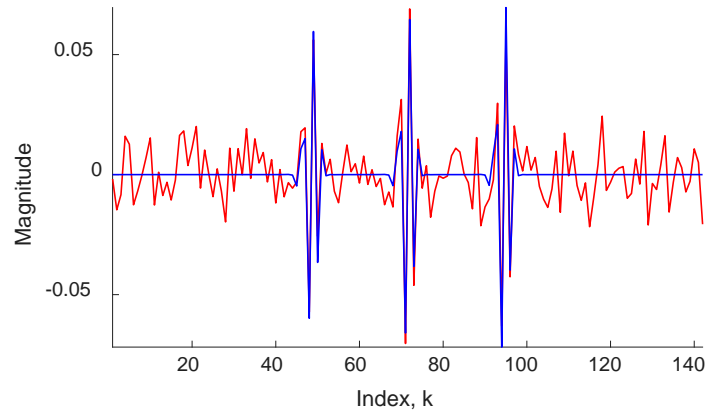
- Signal Magnitude is larger than noise magnitude
- Contribution of Each Detail Component Varies with respect to Input Signal

- Noise-free
- Noisy

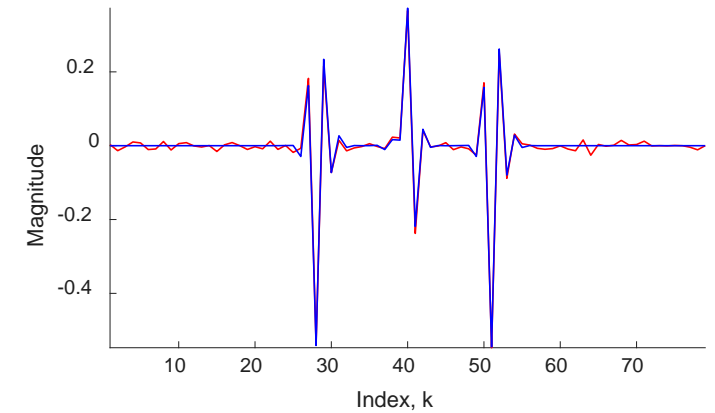
Detail Component with All Noise



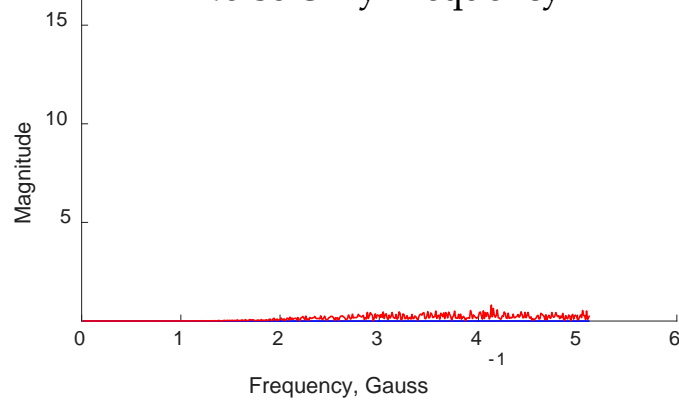
Detail Component with Heavy Noise



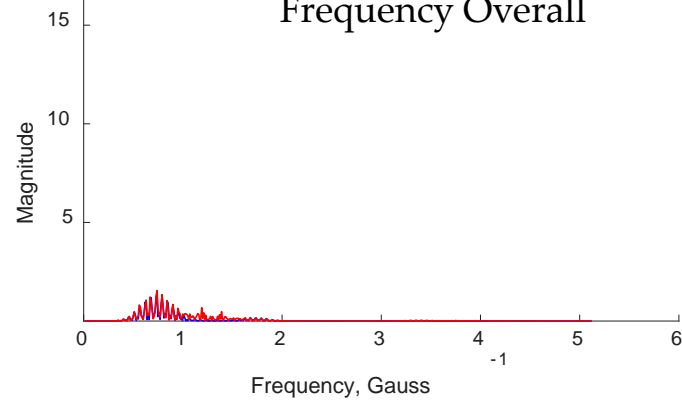
Detail Component with Little Noise



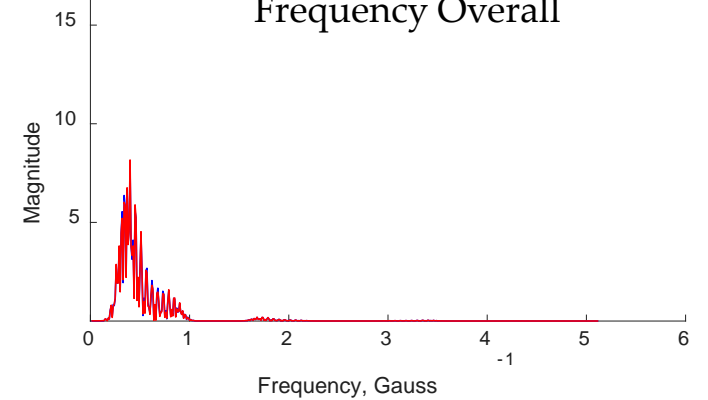
Noise Only Frequency

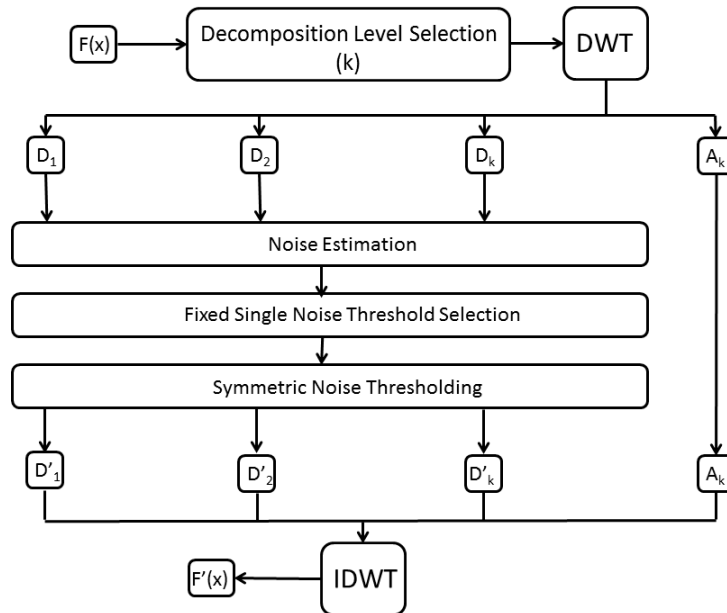


Noise and Signal Frequency Overall



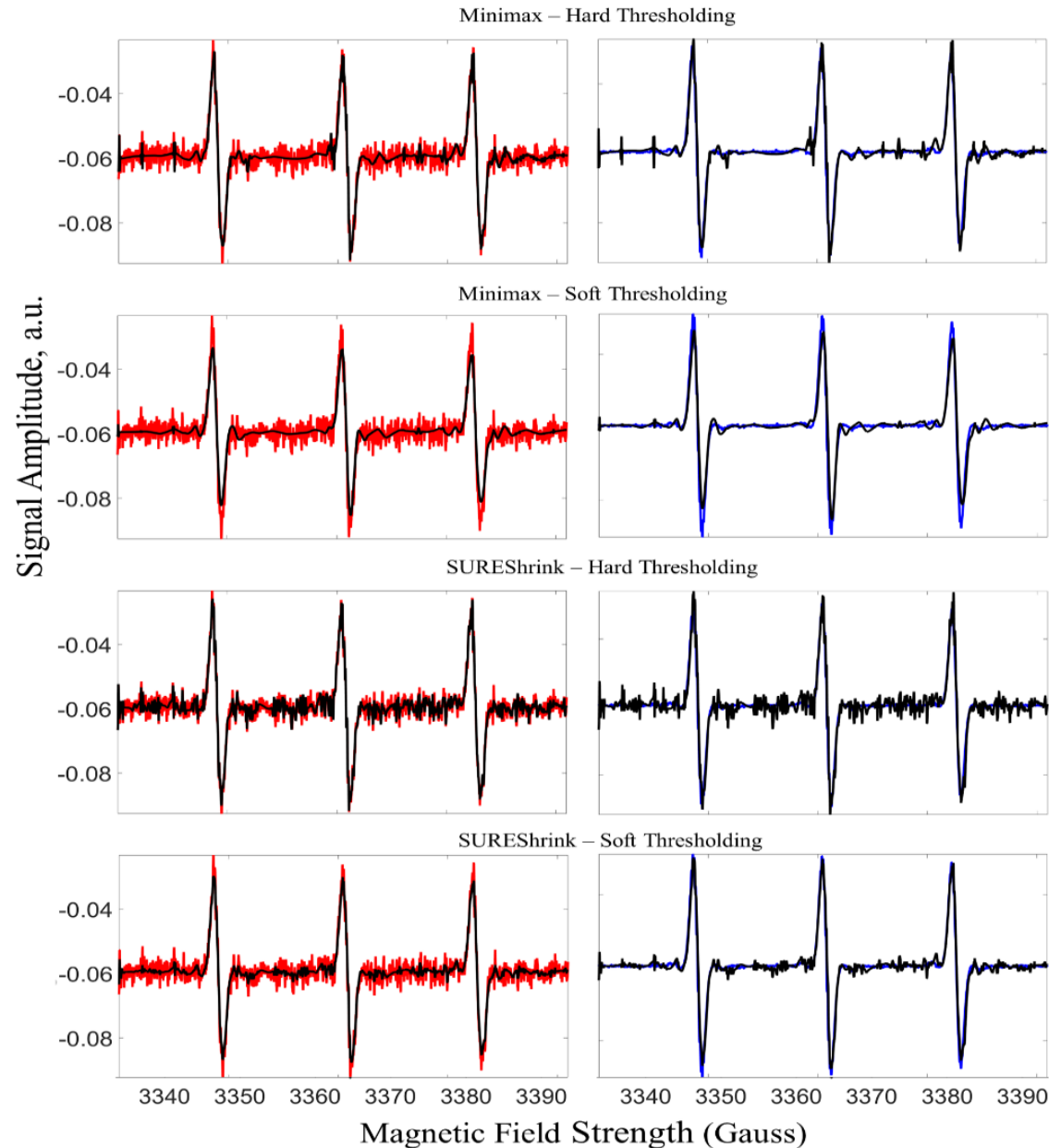
Noise and Signal Frequency Overall



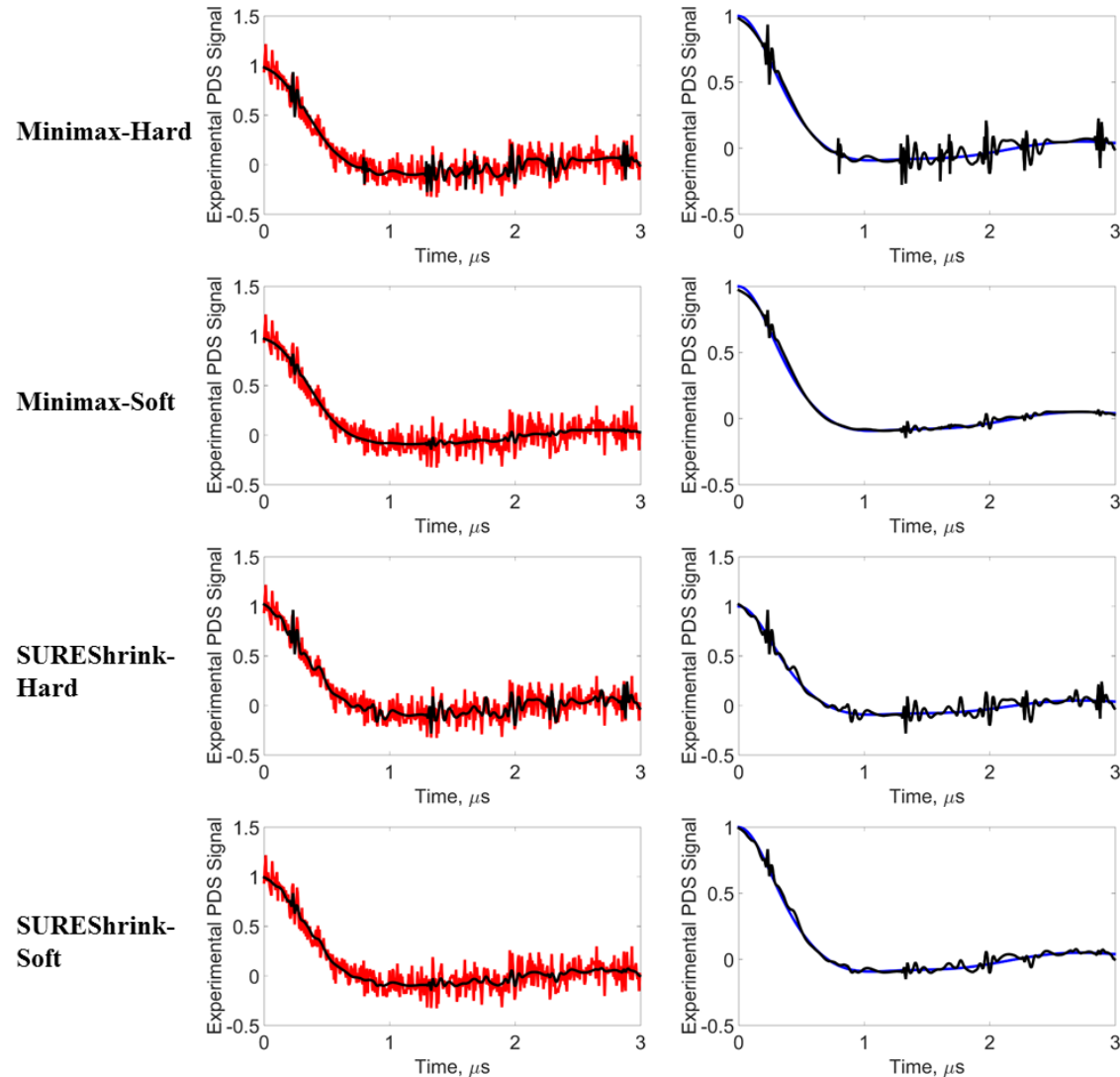


Sequential Steps:

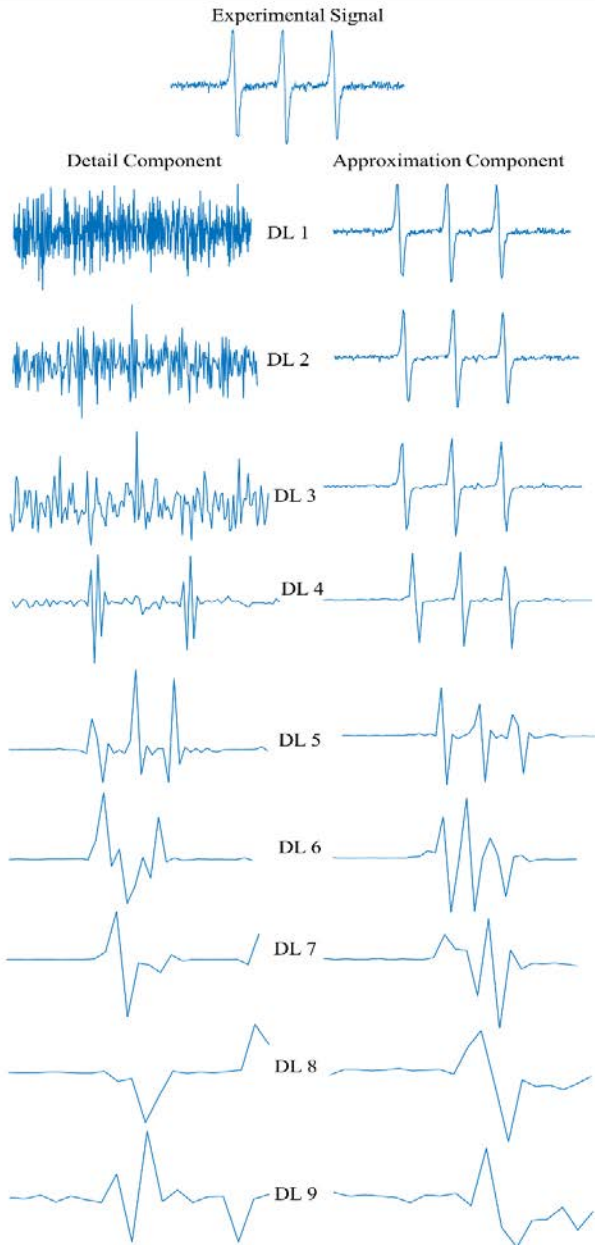
1. Select a wavelet.
2. Select Detail components to denoise.
3. Estimate noise in each Detail component.
4. Calculate noise threshold at each Detail component.
5. Apply noise thresholding.
6. Take IDWT



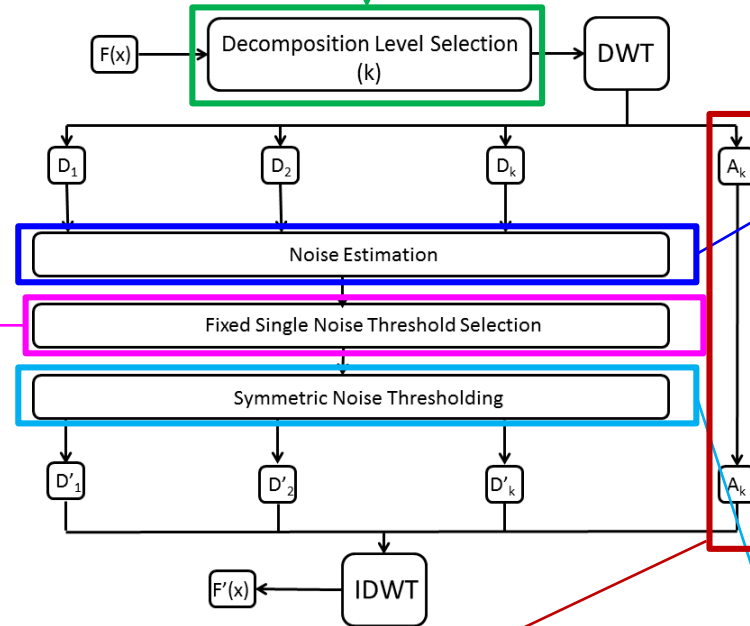
- Reference (500 scans)
- Denoised (4 scans)
- Noisy (4 scans)



- Model
- Denoised
- Noisy



No criteria: Arbitrary selection of decomposition level for denoising, influencing the outcome.



No definitive way to estimate noise; different noise estimates yield different noise thresholds.

Different noise levels can have same median absolute deviation.

$$\eta_j = \frac{MAD(|D_j|)}{0.6745}$$

$$\eta_j = \frac{MAD(|D_1|)}{0.6745}$$

Single threshold for negative and positive coefficients. Assumes no bias.

Noise thresholds are not based on information in Detail components, but on its length.

Non-adjustable thresholds to remove coherent noise or to separate weak signal coefficient from nearby strong noise coefficient.

$$\lambda_j = \eta_j \sqrt{2 \log_2 p_j}$$

Relies on single threshold to remove noise for positive and negative coefficients, resulting in keeping noise coefficients and/or distortion signal.

Soft-thresholding:

$$D'_j[i] = \begin{cases} \text{sgn}(D_j[i]) (|D_j[i]| - \lambda_j) & : |D_j[i]| \geq \lambda_j \\ 0 & : |D_j[i]| < \lambda_j \end{cases}$$

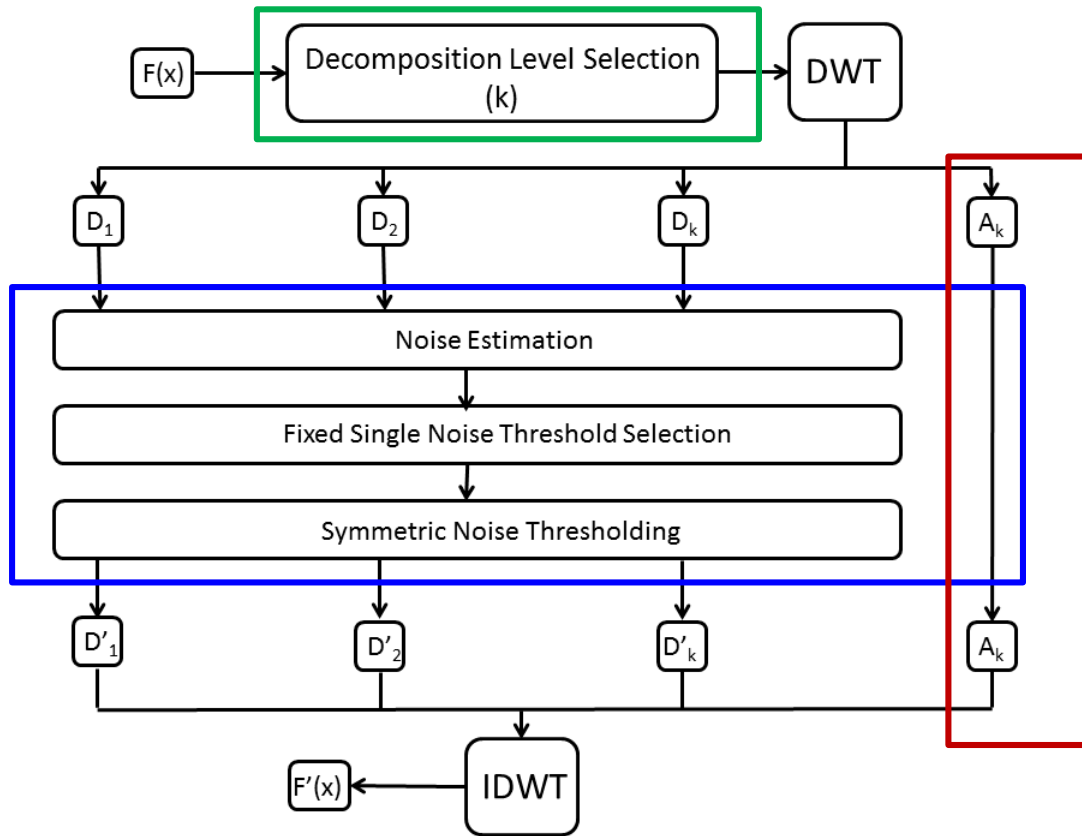
Hard-thresholding:

$$D'_j[i] = \begin{cases} D_j[i] & : |D_j[i]| \geq \lambda_j \\ 0 & : |D_j[i]| < \lambda_j \end{cases}$$

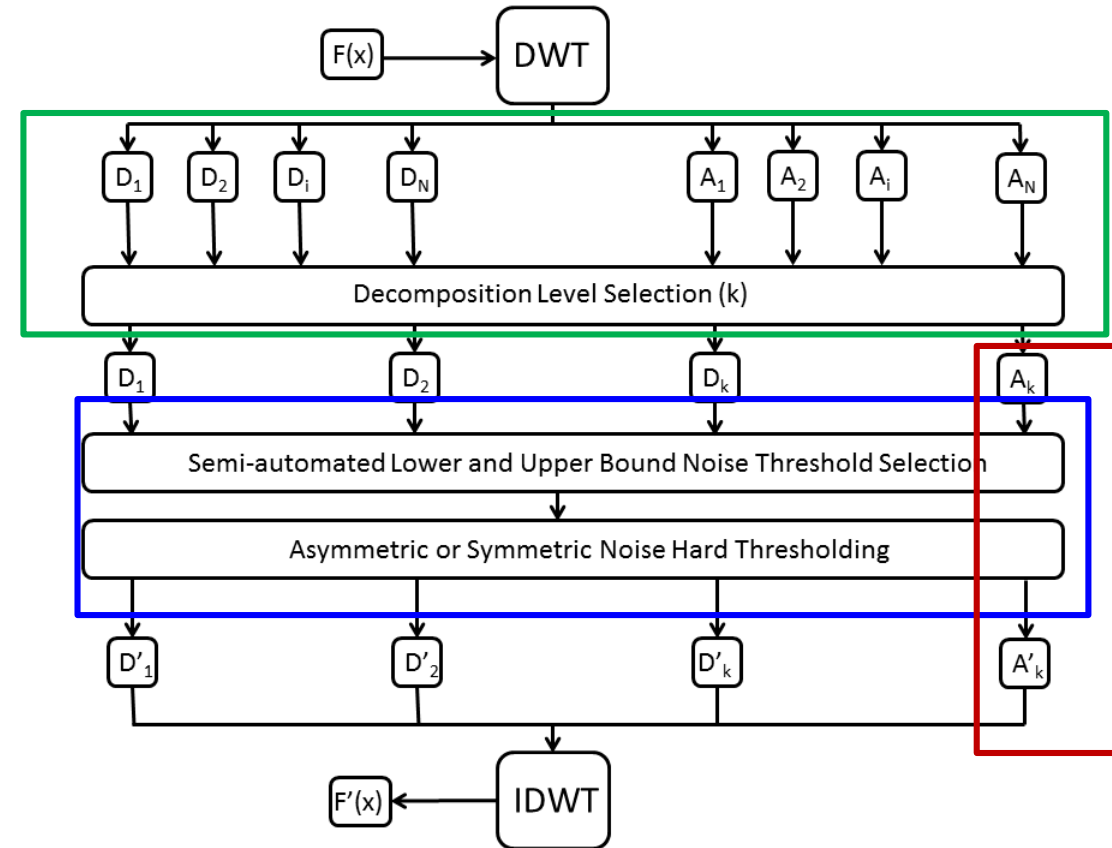
Not removing low frequency noise

- Provides a method to select the number of decomposition levels to denoise
- Uses a new formula to calculate noise thresholds that does not require noise estimation
- Uses separate noise thresholds for positive and negative wavelet coefficients
- Applies denoising to the approximation component
- Allows flexibility for adjusting the noise thresholds

Standard Method



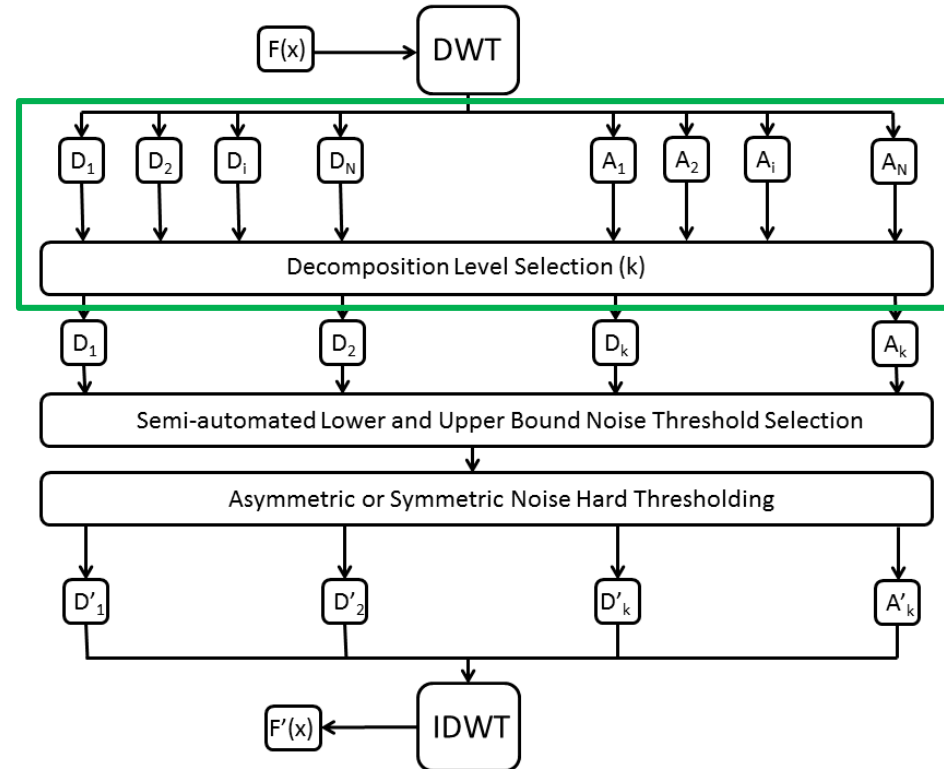
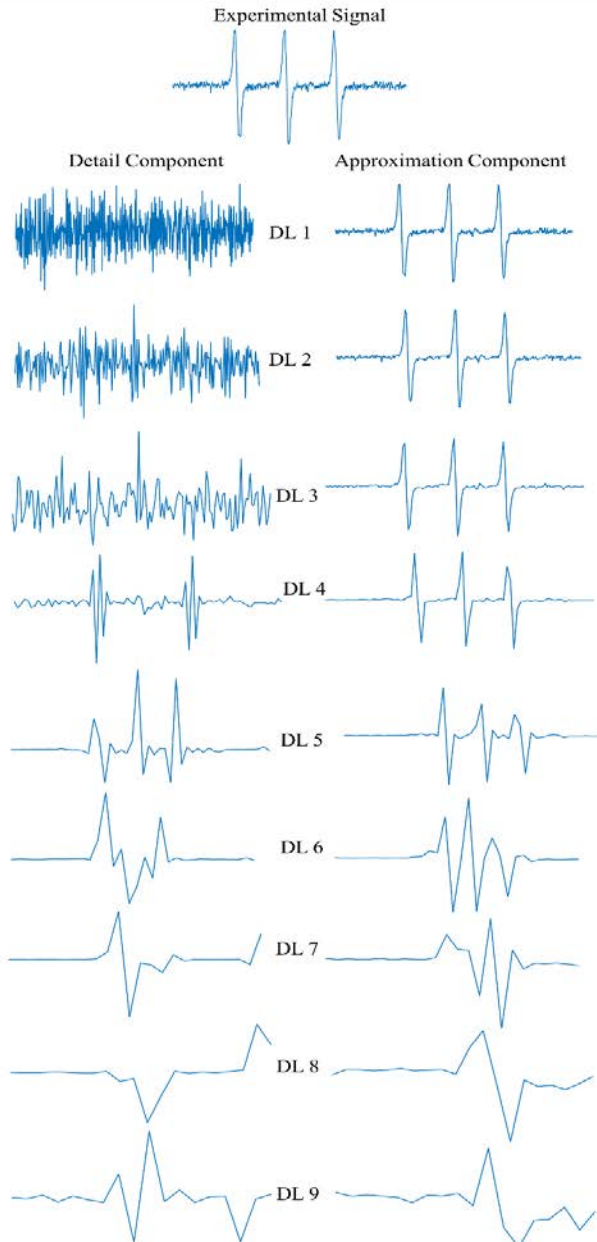
New Method*



1. Decomposition Level Selection Criteria
2. New Noise Threshold Procedure
3. Removing Low Frequency Noise

*USPTO Patent Application # 62/334,626;

Srivastava, Anderson, Freed (2016) *IEEE Access*



1) Subjective Method:

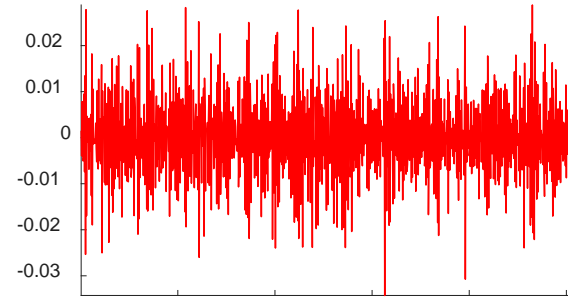
Examine Detail components!

2) Objective Method:

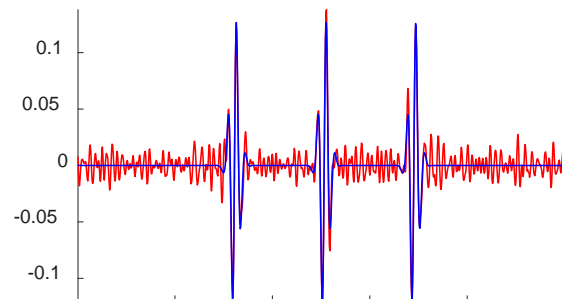
$$S_j = \frac{\max(|D_j[i]|)}{\sum_{k=1}^{p_j} |D_j[i]|}$$

S_j reflects the **sparsity of a wavelet component** allowing the **assessment of noise presence**.

Noise-Only Components (D)



Signal Components with Noise Presence (D)



Noise Threshold Selection

$$\lambda_{j,L} = \mu_j - \kappa_{j,L}\sigma_j$$

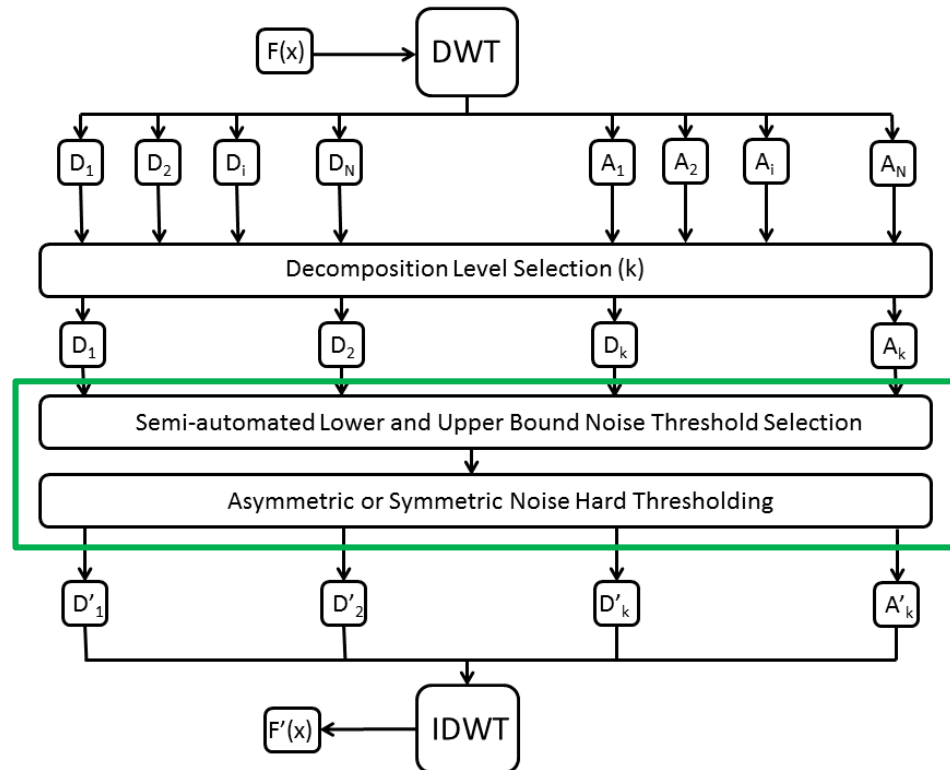
$$\lambda_{j,H} = \mu_j + \kappa_{j,H}\sigma_j$$

Two noise thresholds compared to **single noise threshold in standard method** which distinguishes **positive and negative** noise components.

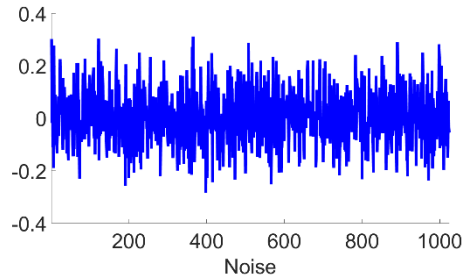
Noise Thresholding:

$$D'_j[i] = \begin{cases} 0, & \lambda_{j,L} \leq D_j[i] \leq \lambda_{j,H} \\ D_j[i], & \text{otherwise} \end{cases}$$

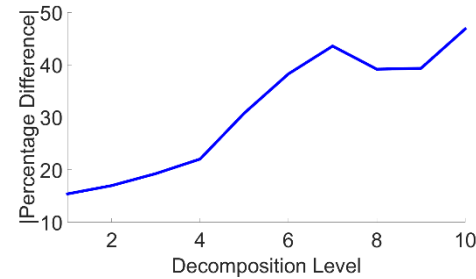
Hard thresholding over **soft thresholding used in standard method**.



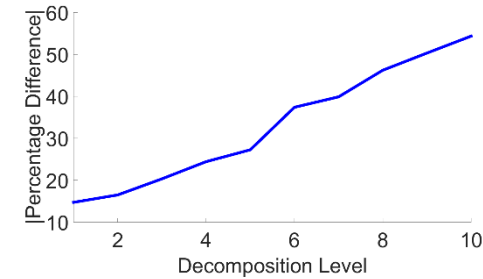
SNR 10



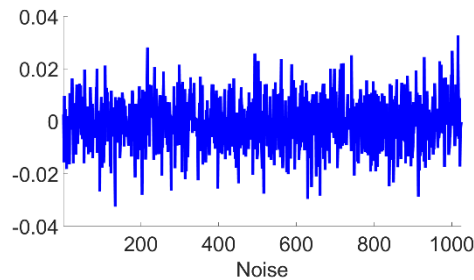
coif 3



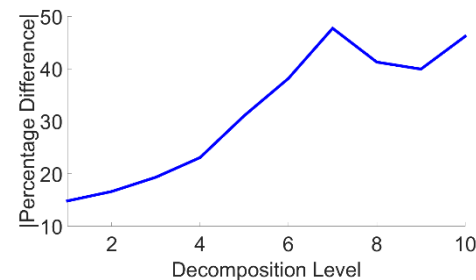
db6



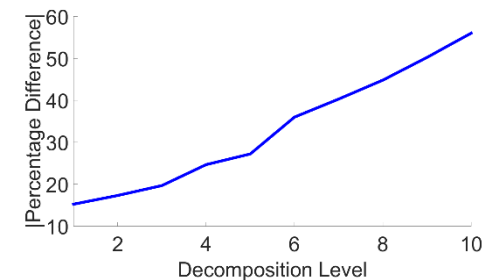
SNR 100



coif 3



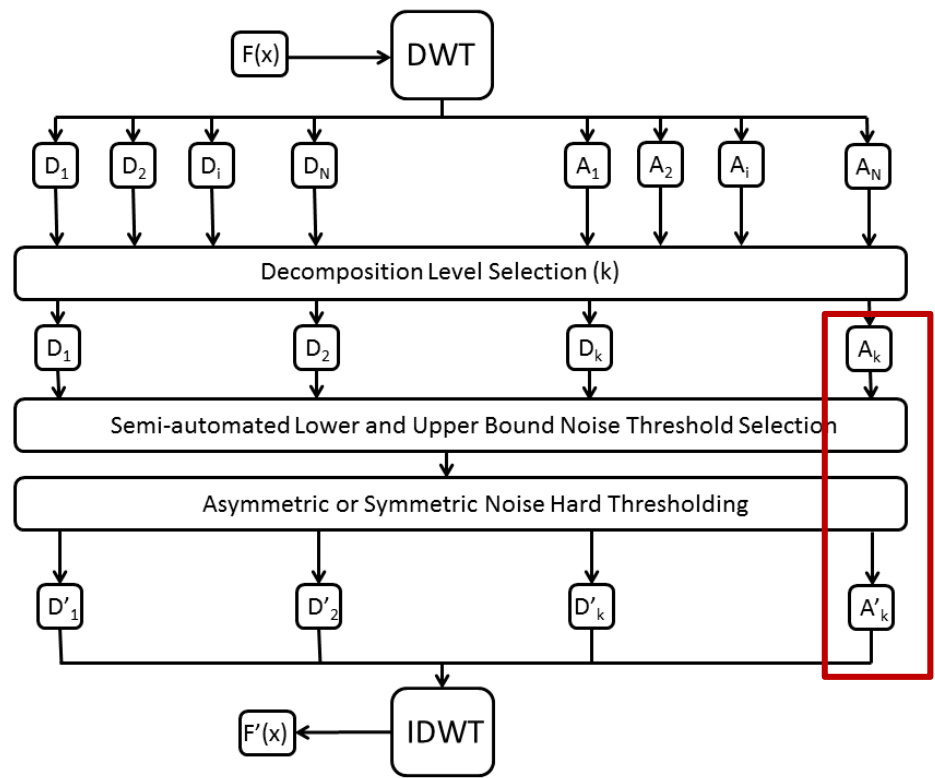
db6



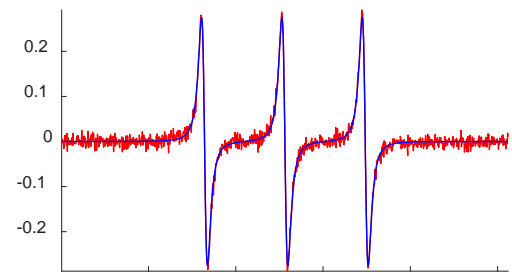
5000 simulations average

Non-Gaussian after WT because of separating Gaussian sub-bands

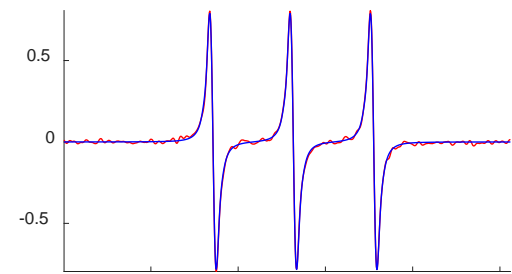
- Noise-free
- Noisy



Noisy Signal at SNR 30



Approximation Component (A_k)



Noise Threshold Selection

$$\lambda_{j,L} = \mu_j - \kappa_{j,L}\sigma_j$$

$$\lambda_{j,H} = \mu_j + \kappa_{j,H}\sigma_j$$

Two noise thresholds

Noise Thresholding:

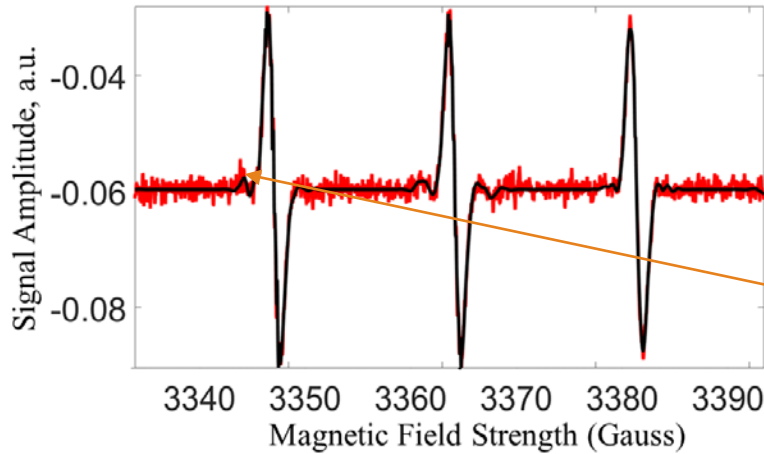
$$A'_j[i] = \begin{cases} 0, & \lambda_{j,L} \leq A_j[i] \leq \lambda_{j,H} \\ A_j[i], & \text{otherwise} \end{cases}$$

Hard thresholding over soft thresholding used in standard method.

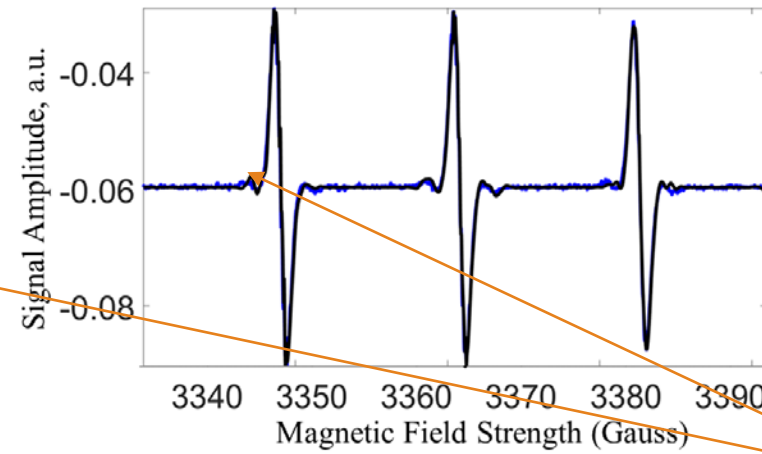
Sample: Tempol, 0.1mM in water at room temperature. X-Band 9.4GHz cw-ESR.

- Noisy
- Reference (500 scans)
- Denoised

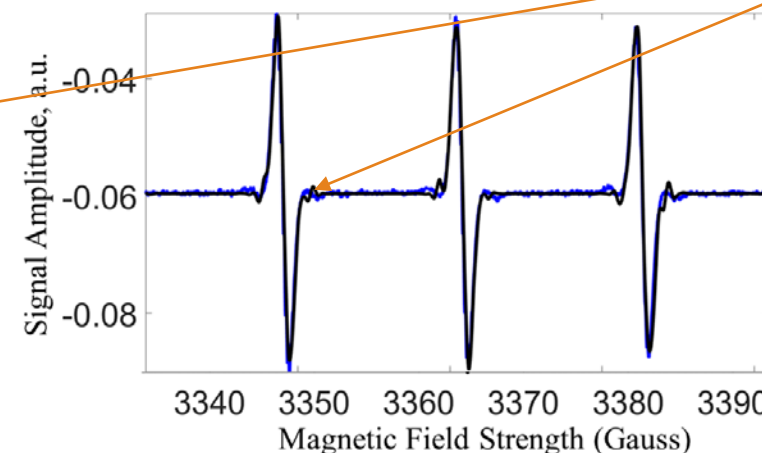
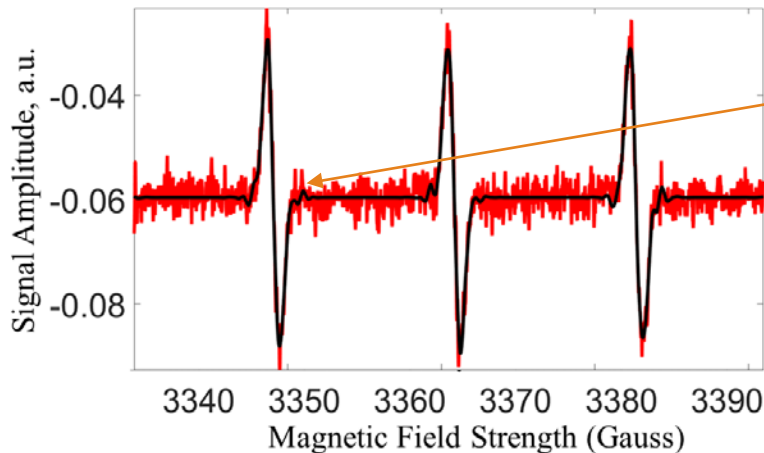
16 Scans



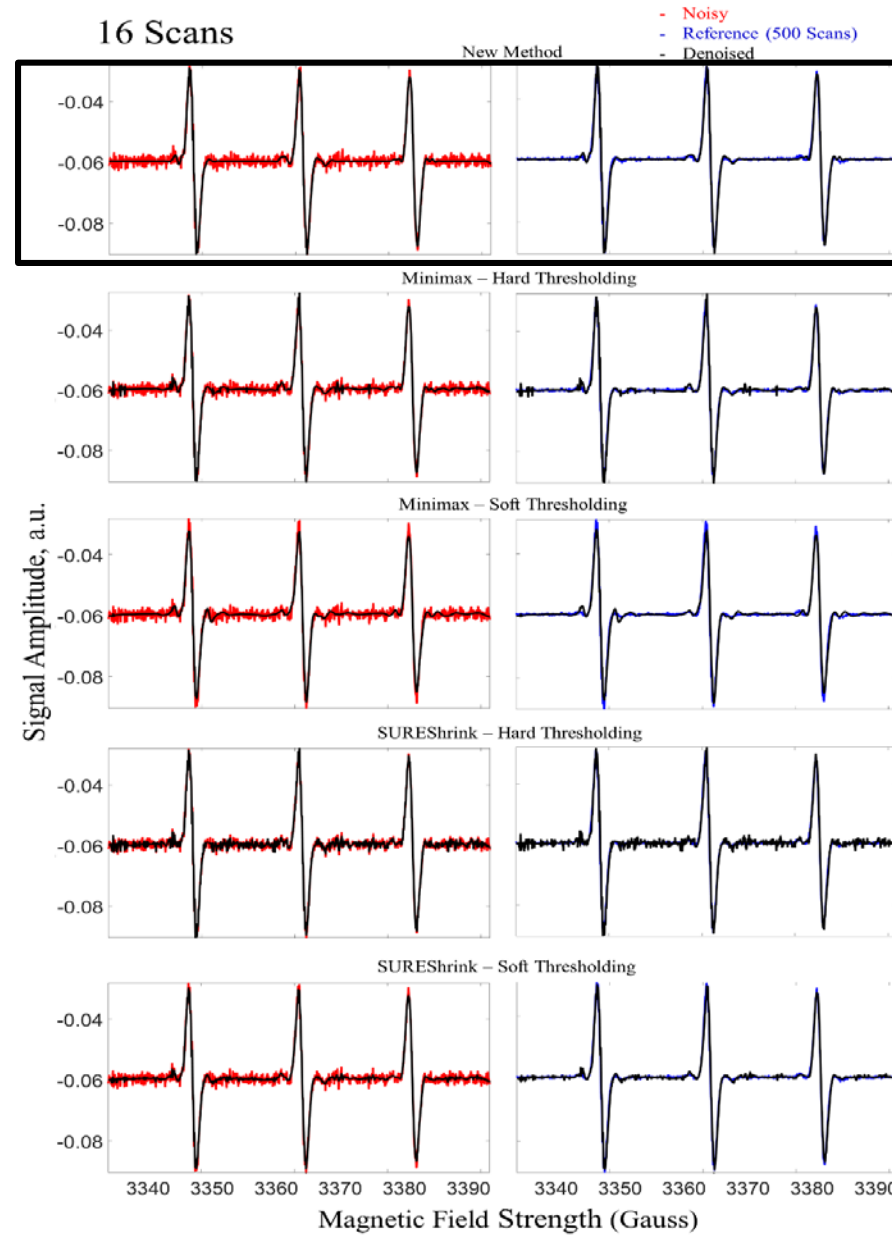
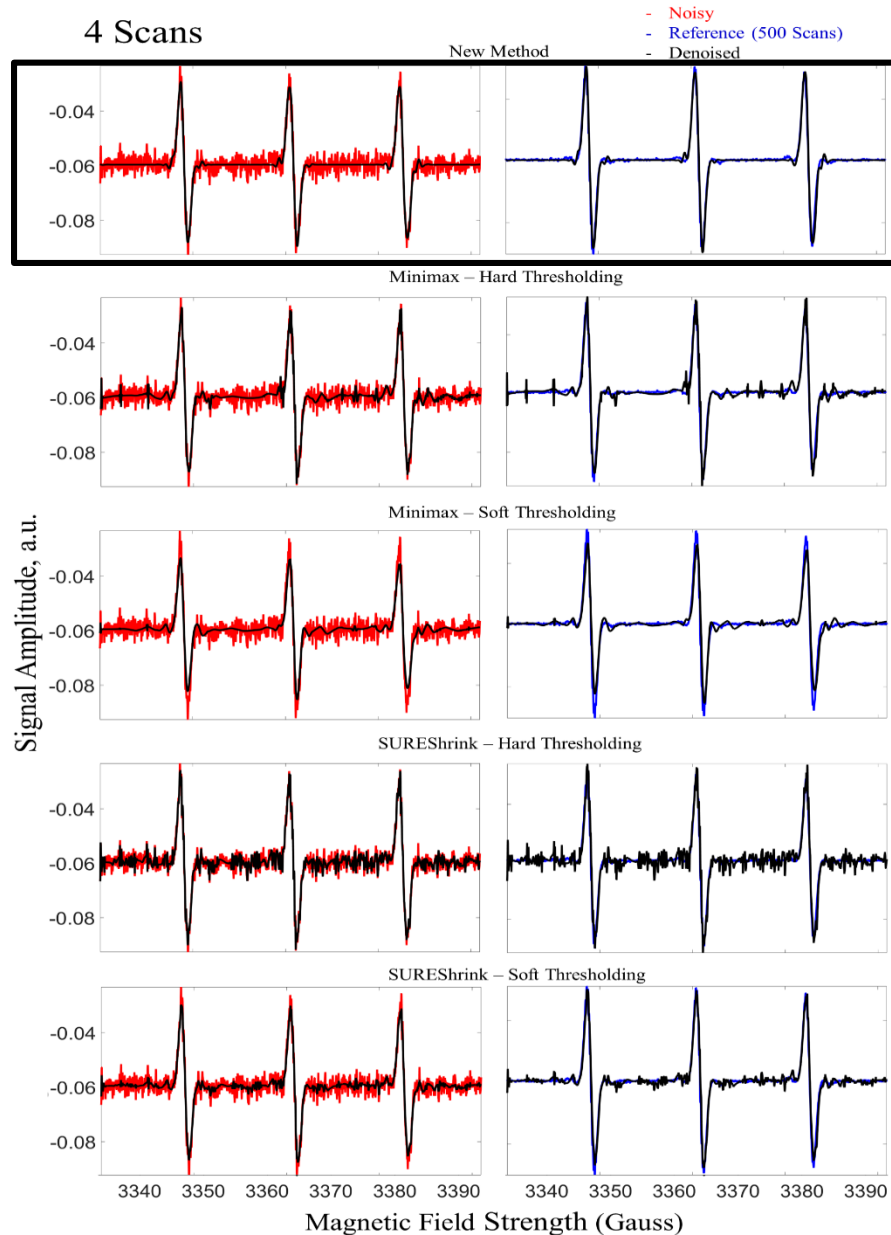
Wavelet: Coiflet 3



4 Scans



Revealing Weak C-13 Peaks



- Noisy
- Reference (500 scans)
- Denoised

Sample: Tempol, 0.1mM in water at room temperature.
X-Band 9.4GHz cw-ESR.

Method	4 scans				16 scans			
	SNR	SSIM	DL	CT(s)	SNR	SSIM	DL	CT(s)
Noisy	14	0.9684	-	-	30	0.9903	-	-
Minimax-Hard	40	0.9880	7	0.0834	73	0.9959	7	0.0804
Minimax-Soft	57	0.9890	12	0.0788	100	0.9954	7	0.0807
SUREShrink-Hard	20	0.9779	9	0.0878	41	0.9938	9	0.0853
SUREShrink-Soft	39	0.9905	12	0.0866	79	0.9966	7	0.0873
Zhao	40	0.9790	6	0.0864	104	0.9821	6	0.0864
Poornachandra	36	0.9803	6	0.0849	84	0.9825	6	0.0857
Zhang	40	0.9778	6	0.0855	105	0.9821	6	0.0858
Lin	39	0.9800	6	0.0852	134	0.9825	6	0.0867
<i>New Method</i>	784	0.9957	6	0.0140	2220	0.9969	6	0.0131

$$SSIM(X, Y) = \frac{(2\mu_X\mu_Y + c_1)(2\sigma_{XY} + c_2)}{(\mu_X^2 + \mu_Y^2 + c_1)(\sigma_X^2 + \sigma_Y^2 + c_2)}$$

- μ_X = mean of signal X
- μ_Y = mean of signal Y
- σ_X^2 = variance of X
- σ_Y^2 = variance of Y
- σ_{XY} = co-variance of X and Y
- c_1, c_2 = constant terms

* For standard methods, DL that resulted in maximum SNR was selected.

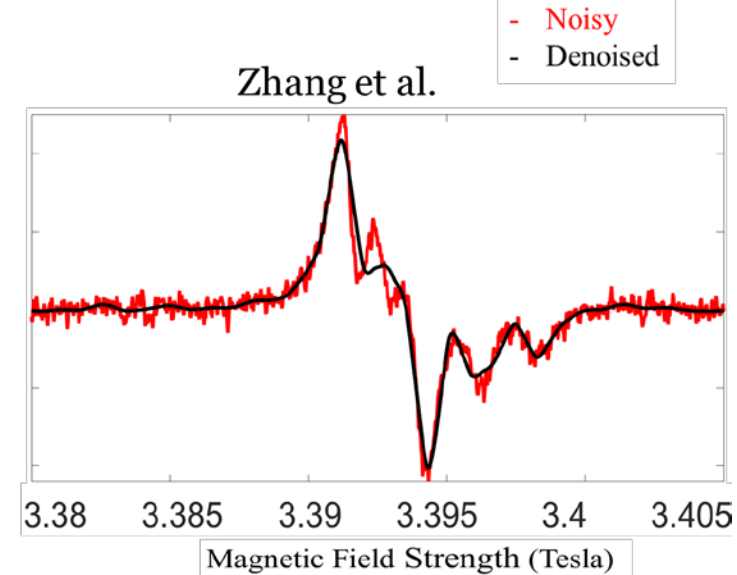
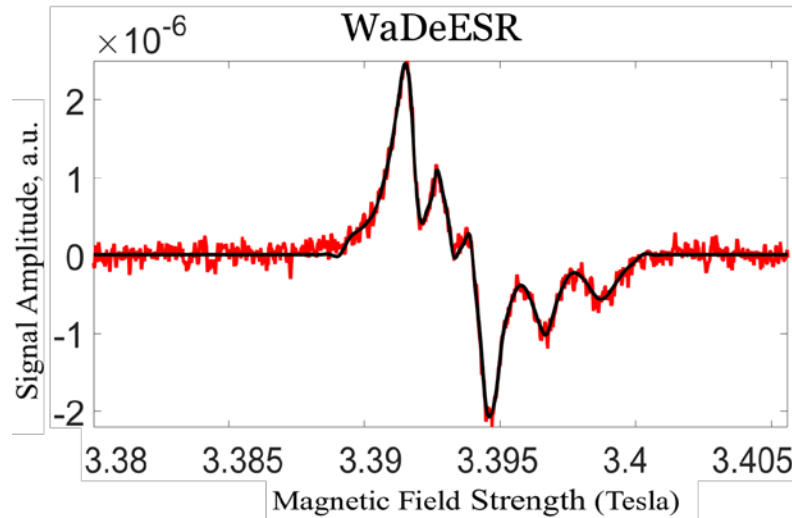
- Hard and Soft is hard and soft thresholding
- SSIM is structural similarity index measure
- DL is decomposition level
- CT is computation time

WaDeESR: Experimental Slow Motion cw-ESR Denoising

Sample: 0.5% lipid spin label 16-PC in lipid vesicles at room temperature. W-band 95 GHz cw-ESR

18 scans

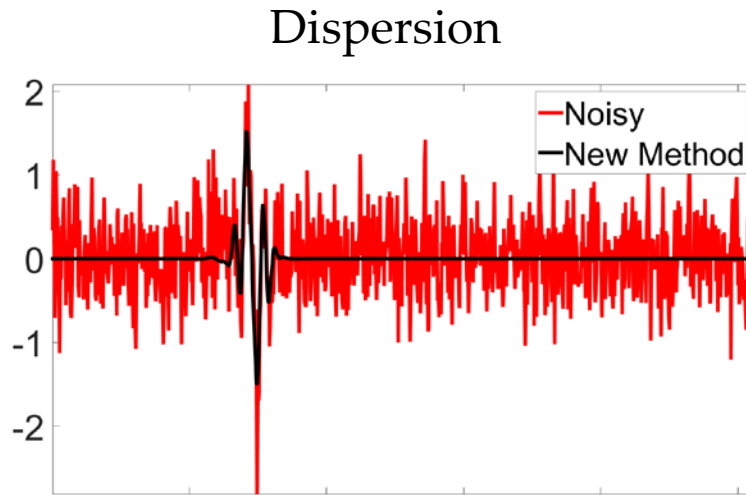
Wavelet: Coiflet 3



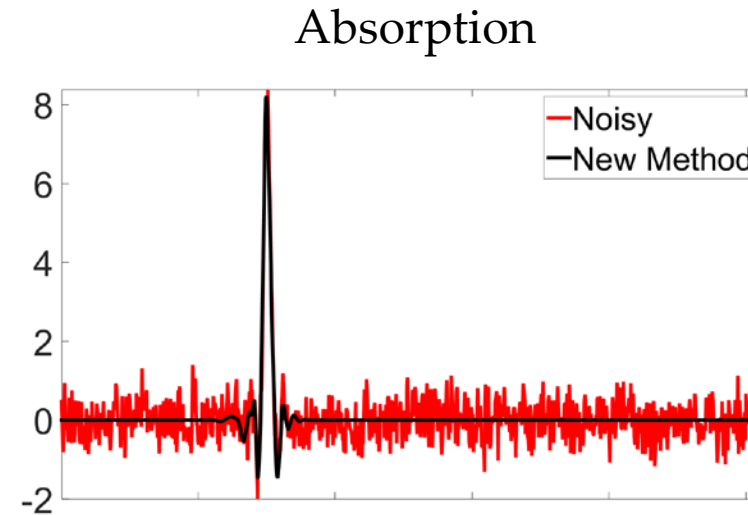
- Noisy
- Denoised

<i>Method</i>	<i>SNR</i>	<i>DL</i>
Noisy	49	-
Minimax-Hard	81	10
Minimax-Soft	149	6
SUREShrink-Hard	76	7
SUREShrink-Soft	115	9
Zhang et al.	167	6
WaDeESR	$191 * 10^6$	4

Wavelet: Coiflet 3



SNR Noisy: 4
SNR Denoised: 1.69×10^7



SNR Noisy: 19
SNR Denoised: 8.96×10^6

Sample: $20 \mu\text{M}$ of a biradical, i.e. $40 \mu\text{M}$ nitroxide spins in the rigid limit. The $\pi/2$ pulses were 2 ns providing full coverage. The signal was phased to find the real part of the signal in the I channel.

Noise Elimination and Reduction via Denoising (NERD)

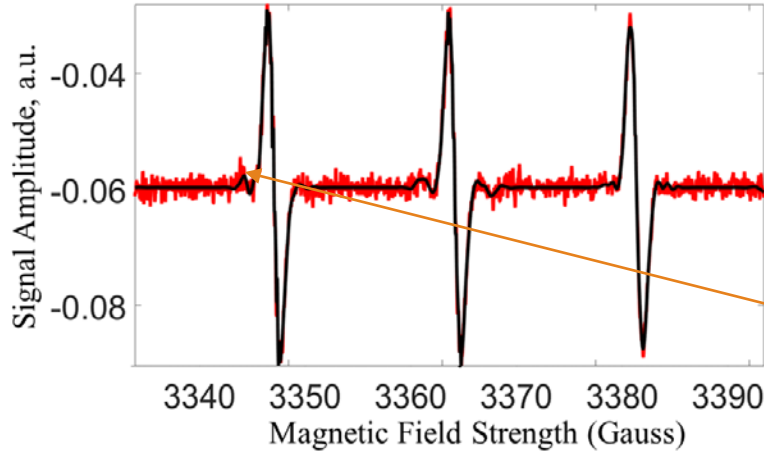
cw-ESR and Other Spectroscopies

- NERD: 1) Replace Decimated by Undecimated Discrete Wavelet Transform
2) Signal Localization during Noise Thresholding

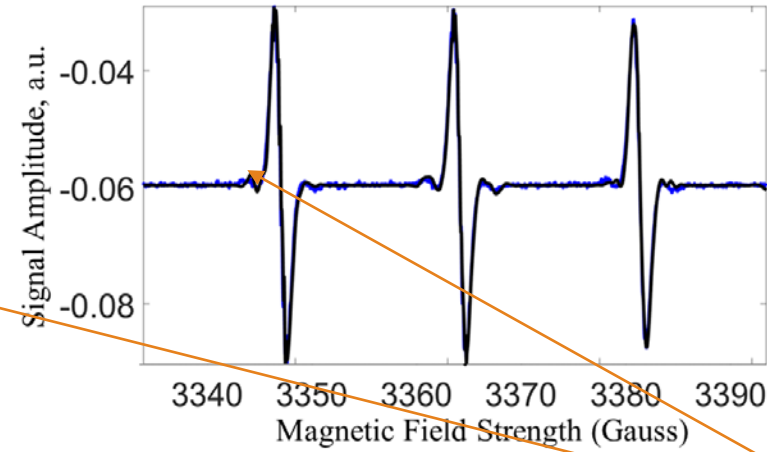
Sample: Tempol, 0.1mM in water at room temperature. X-Band 9.4GHz cw-ESR.

- Noisy
- Reference (500 scans)
- Denoised

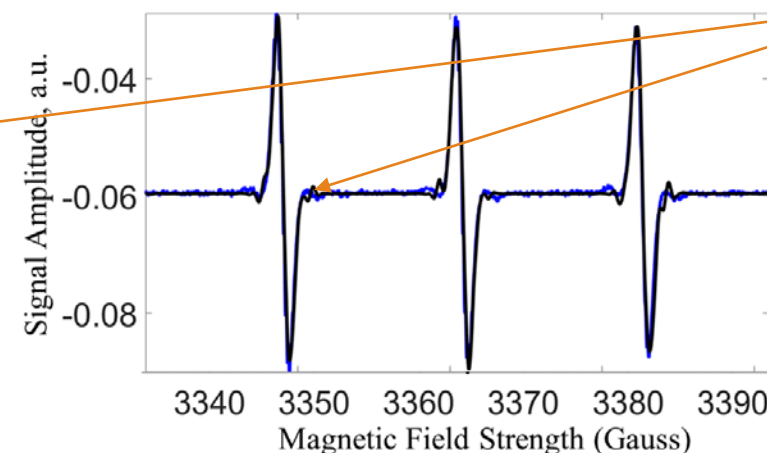
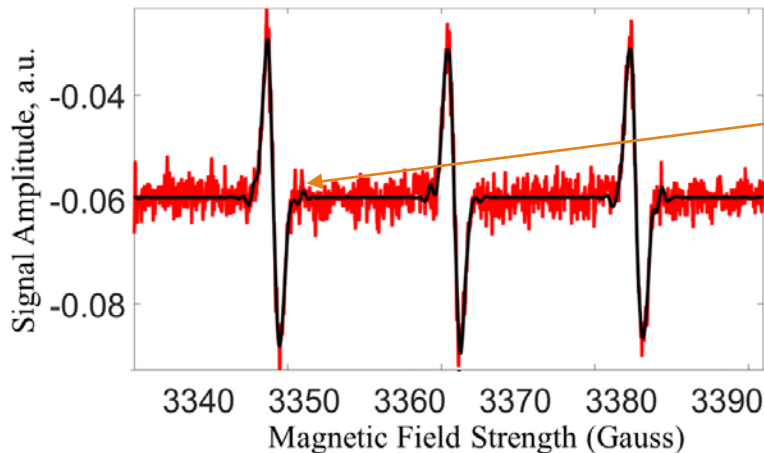
16 Scans



Wavelet: Coiflet 3



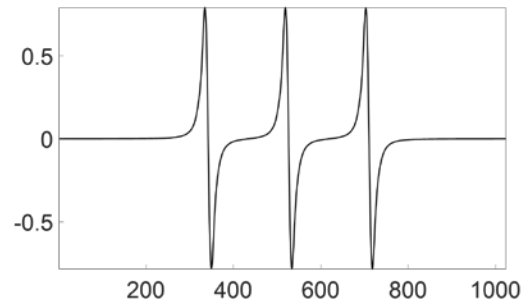
4 Scans



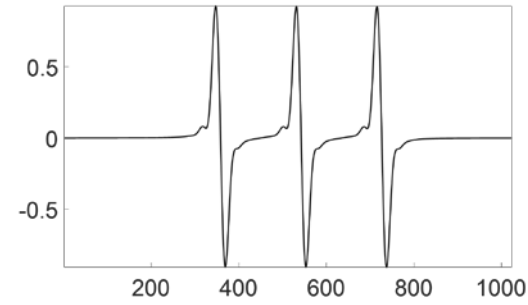
Revealing Weak C-13 Peaks, but needs better resolution

Undecimated DWT

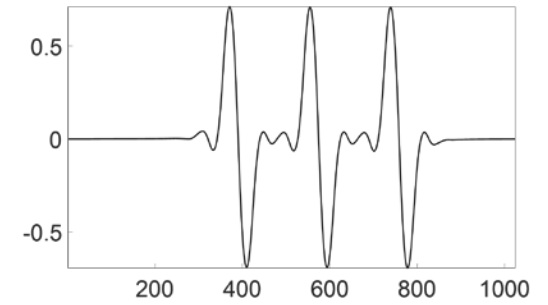
Decomposition Level 3



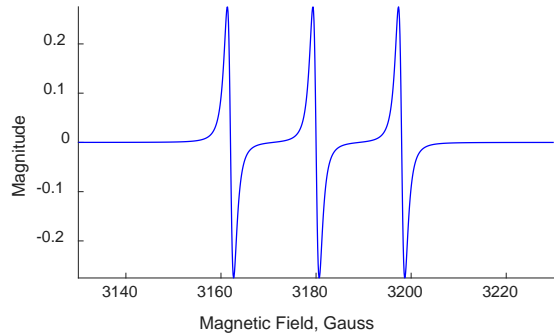
Decomposition Level 4



Decomposition Level 5

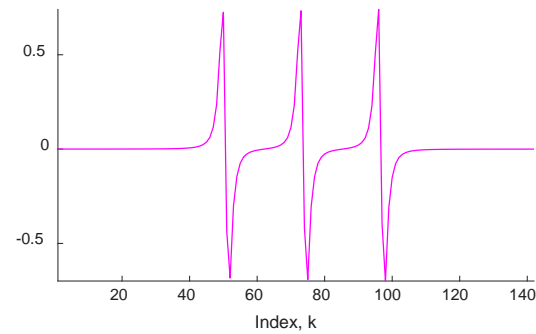


Input Signal

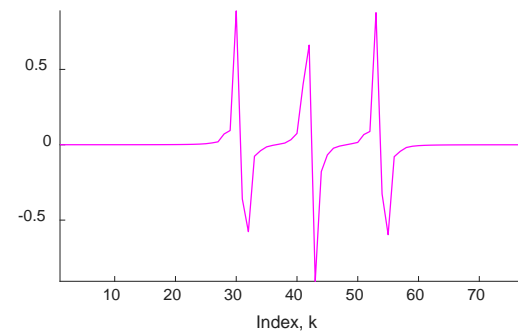


Decimated DWT

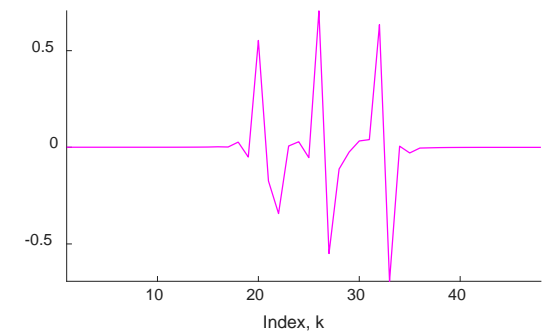
Decomposition Level 3



Decomposition Level 4

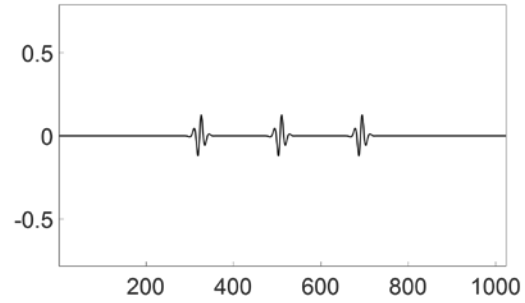


Decomposition Level 5

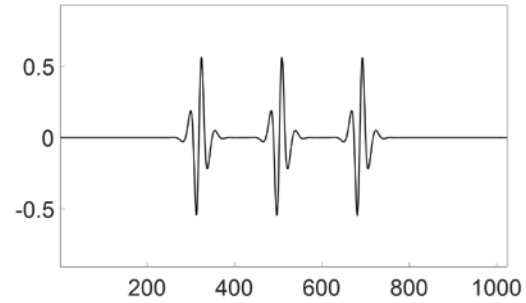


Undecimated DWT

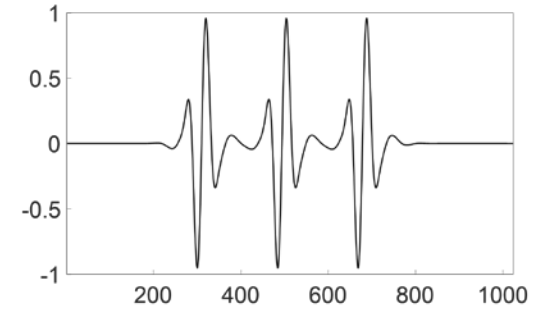
Decomposition Level 3



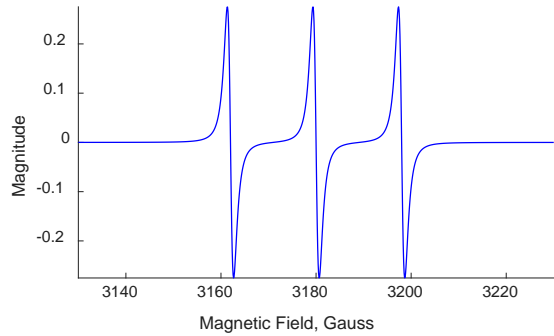
Decomposition Level 4



Decomposition Level 5

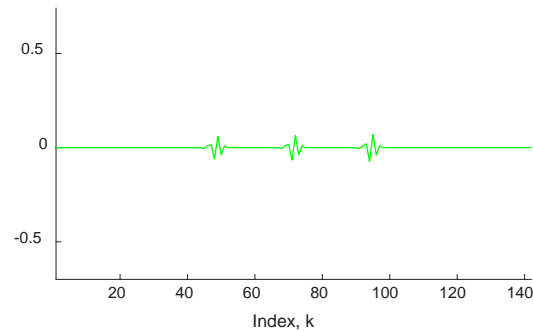


Input Signal

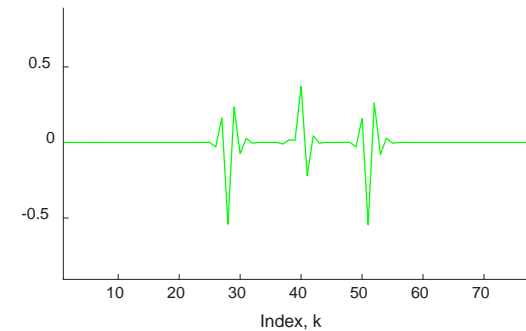


Decimated DWT

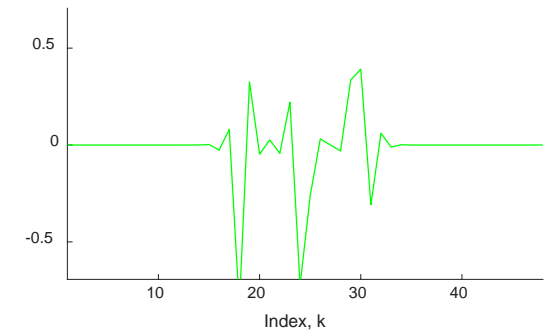
Decomposition Level 3



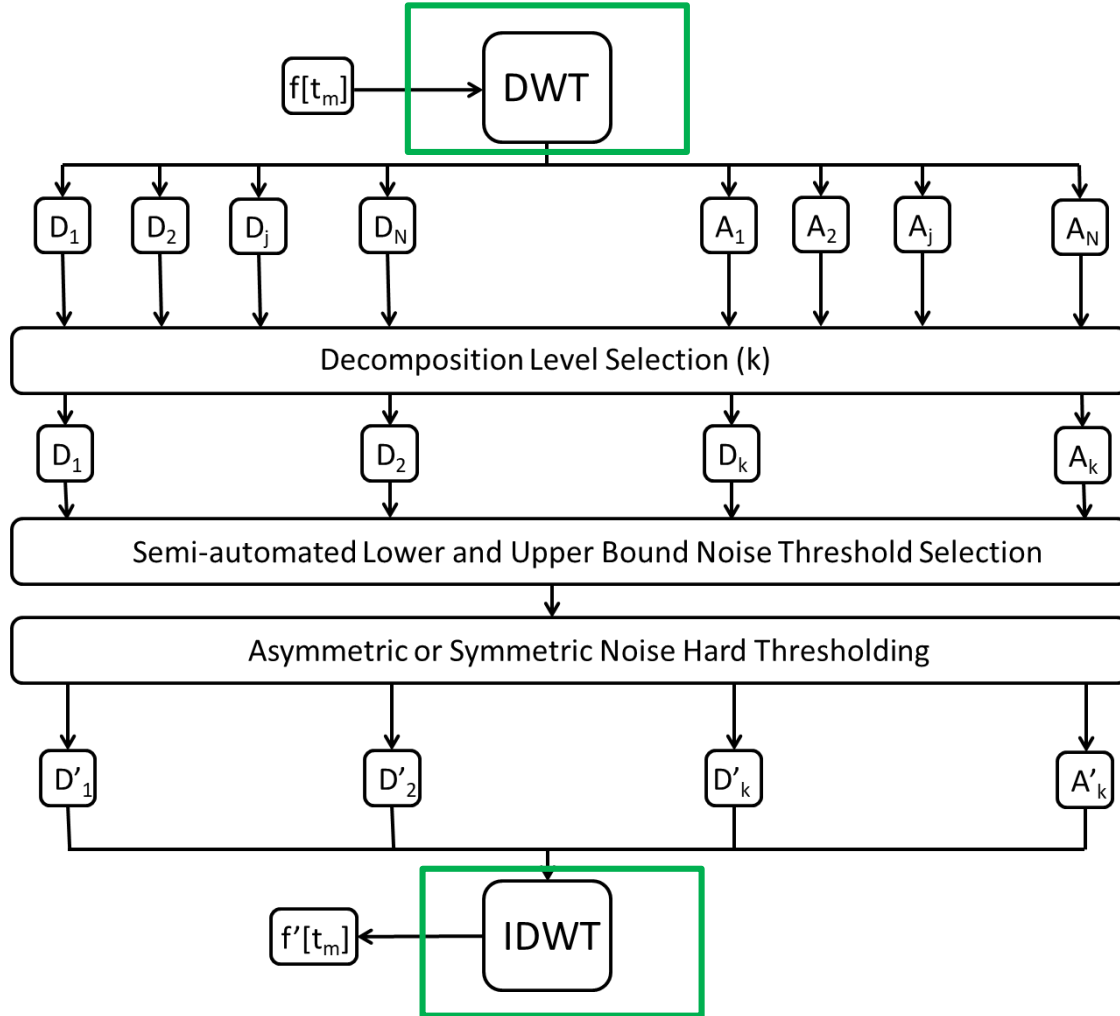
Decomposition Level 4



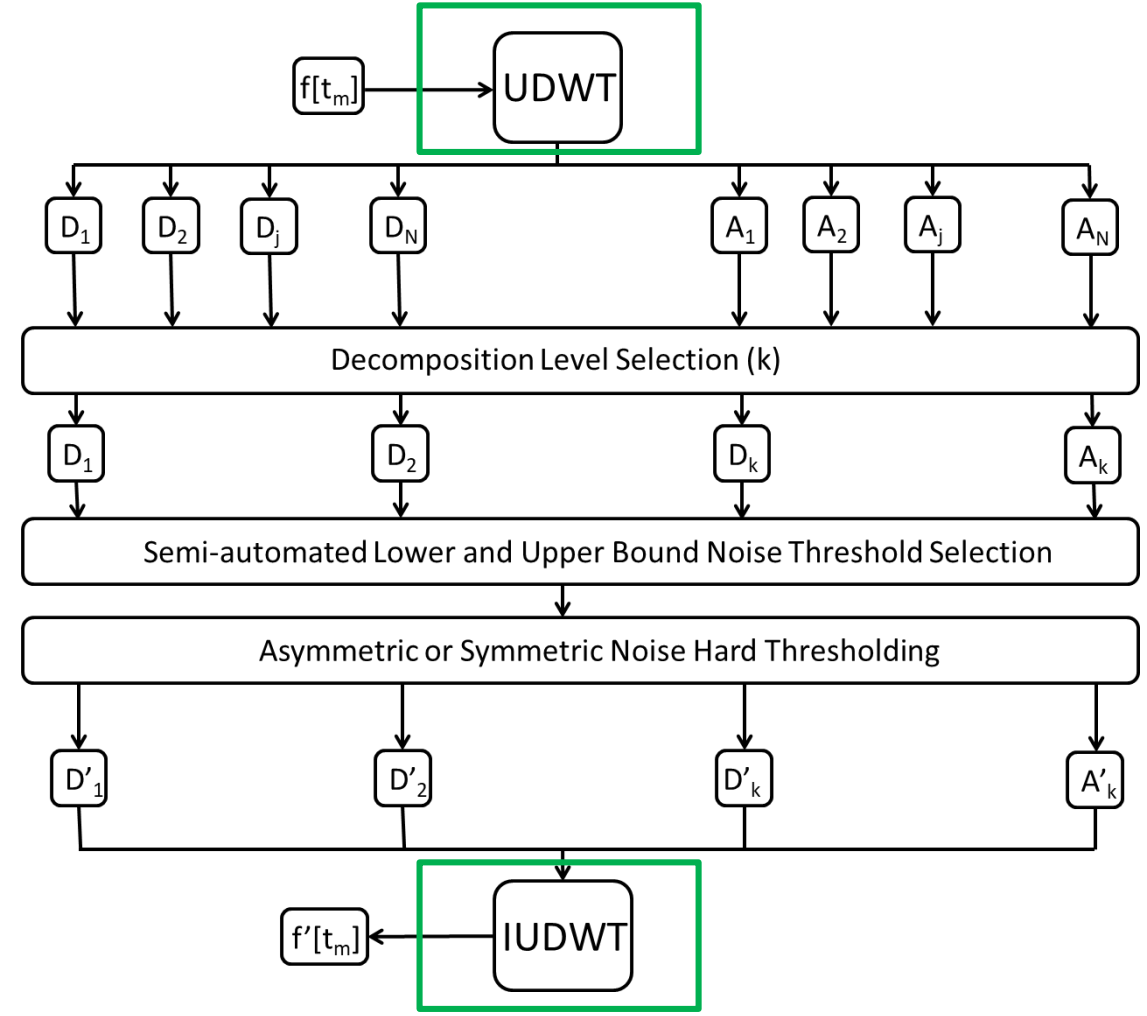
Decomposition Level 5



New Method (IEEE Paper):

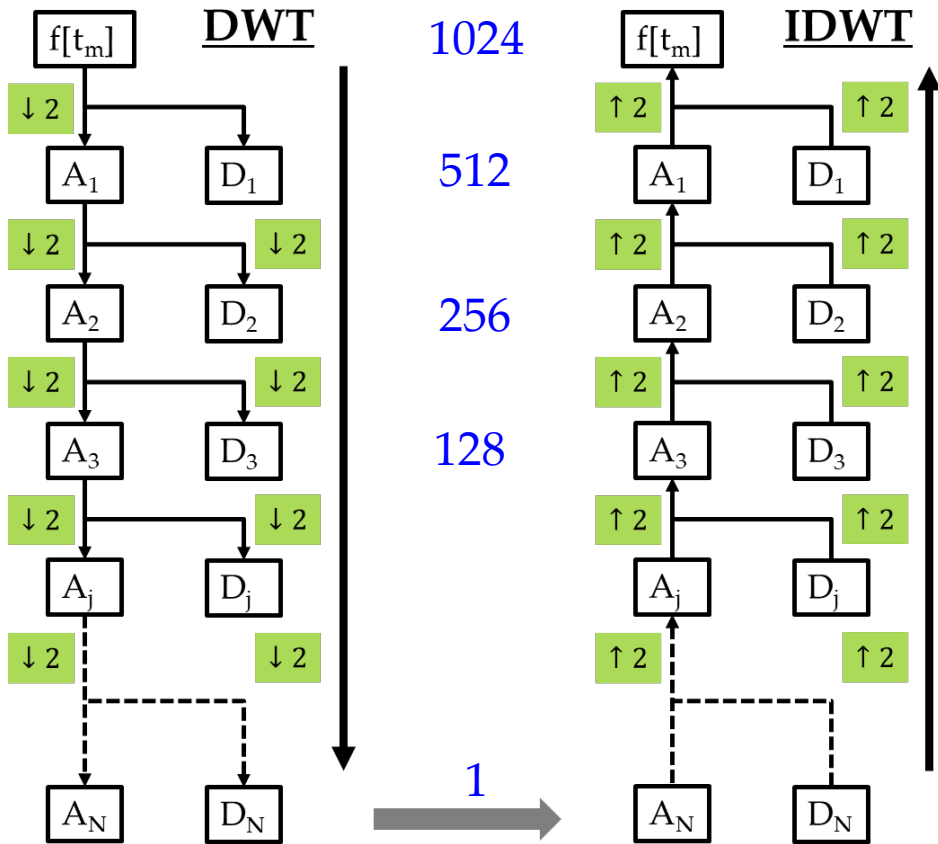


NERD

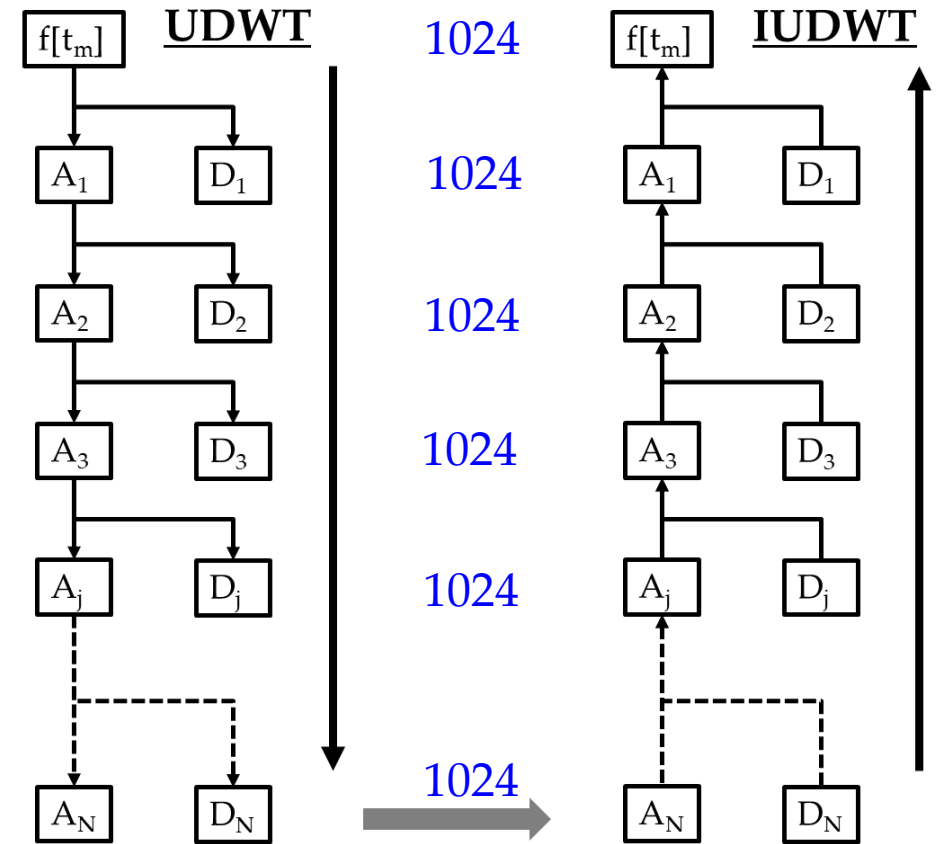


NERD uses Undecimated Discrete Wavelet Transform to improve signal resolution for denoising

Decimated DWT and IDWT

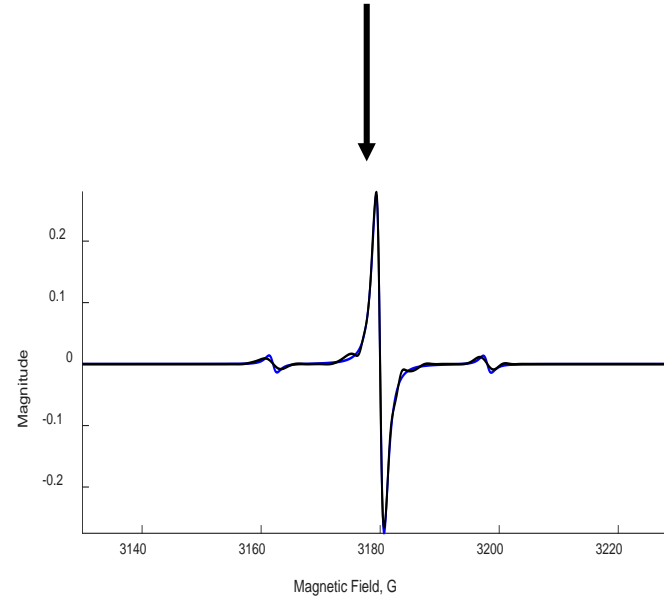
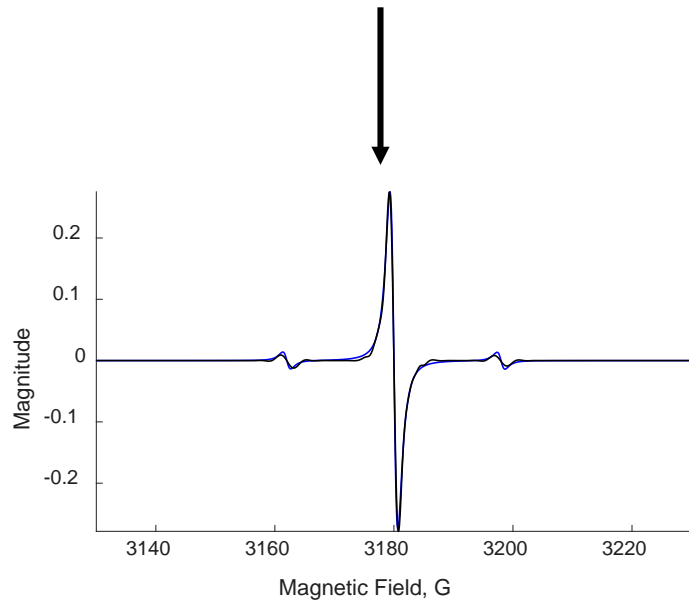
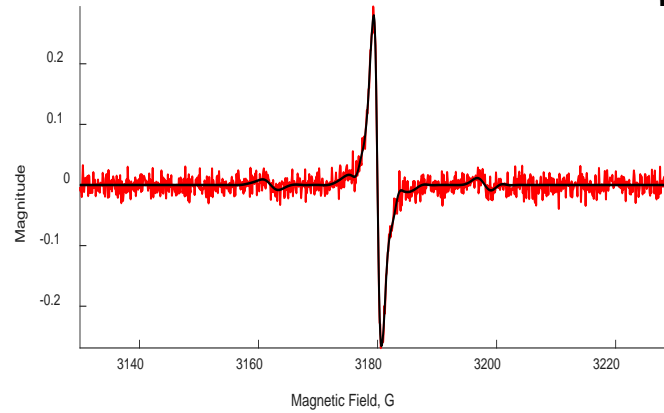
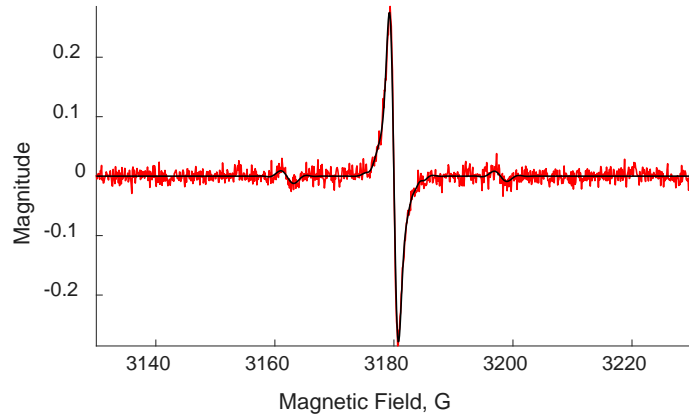


Undecimated DWT and IDWT



$$N = \log_2(\text{SignalLength})$$

- Noisy
- Reference (500 scans)
- ▮ Denoised

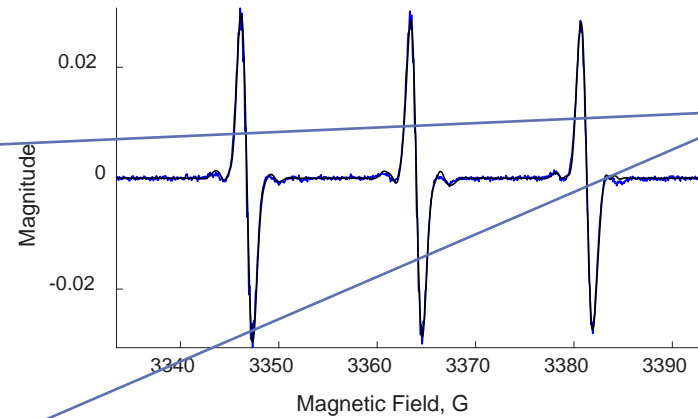
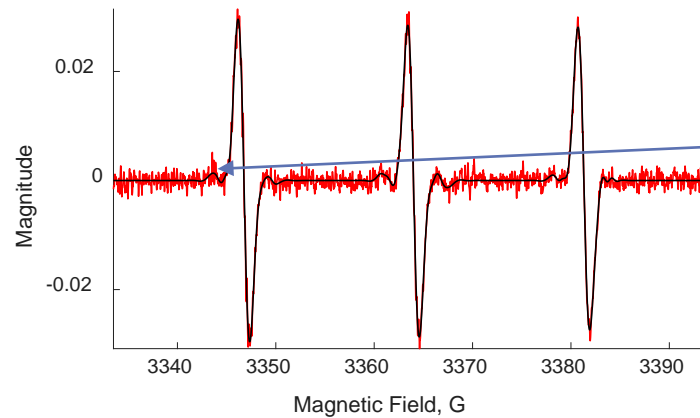


Signal		Noisy SNR	Denoised SNR
Case 1	Main Signal	30	4.36×10^6
	Weak Signal	3	1.91×10^5
Case 2	Main Signal	10	1.99×10^5
	Weak Signal	1	4.70×10^3

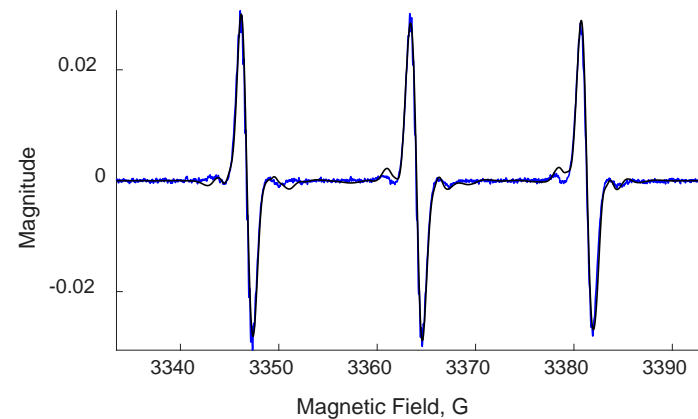
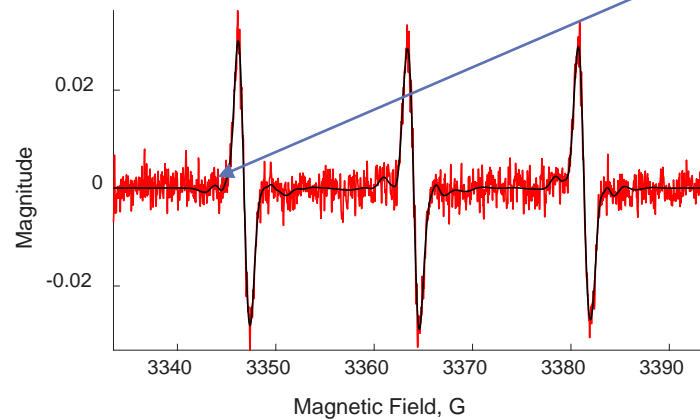
Sample: Tempol, 0.1mM in water at room temperature. X-Band 9.4GHz cw-ESR.

- **Noisy**
- **Reference (500 scans)**
- **Denoised**

16 Scans



4 Scans



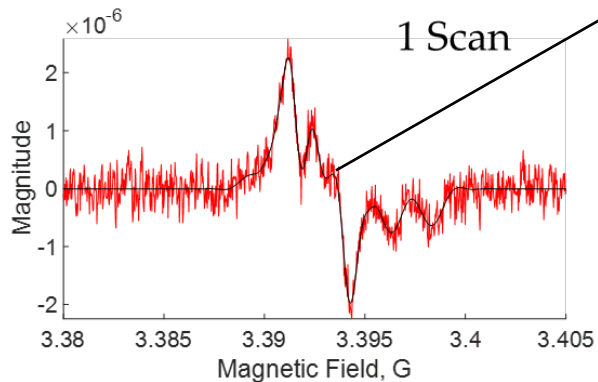
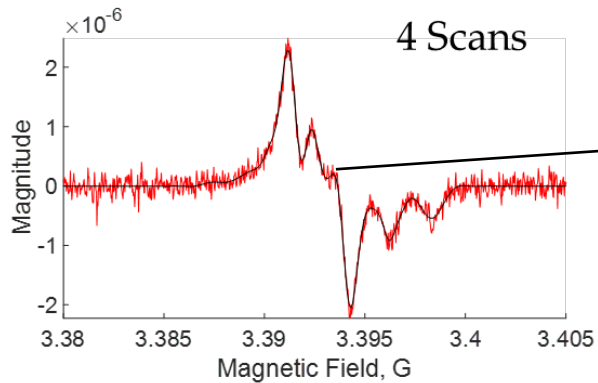
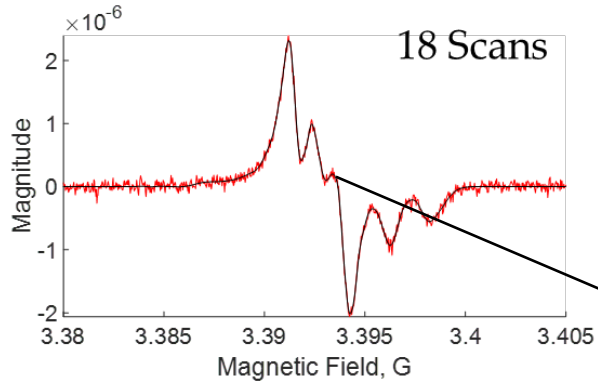
Wavelet: Coiflet 3

Revealing Weak C-13 Peaks

Signal		Noisy SNR	Denoised SNR
16 Scans	Main Signal	30	46416
	Weak Signal	1.5	1613
4 Scans	Main Signal	14	2435
	Weak Signal	0.5	85

Wavelet: Coiflet 3

Sample: 0.5% lipid spin label 16-PC in lipid vesicles at room temperature. W-band 95 GHz cw-ESR

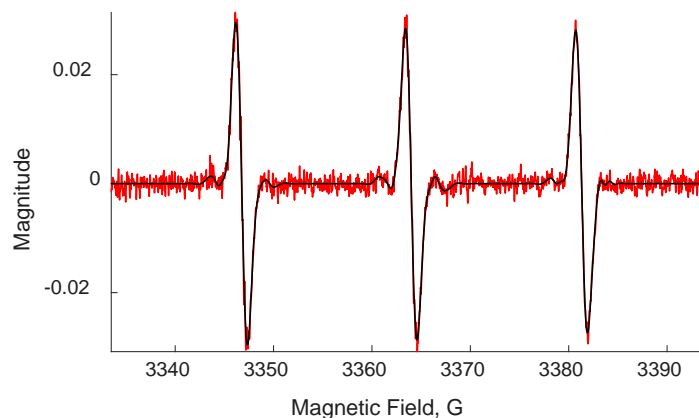


Hidden Peaks Extracted

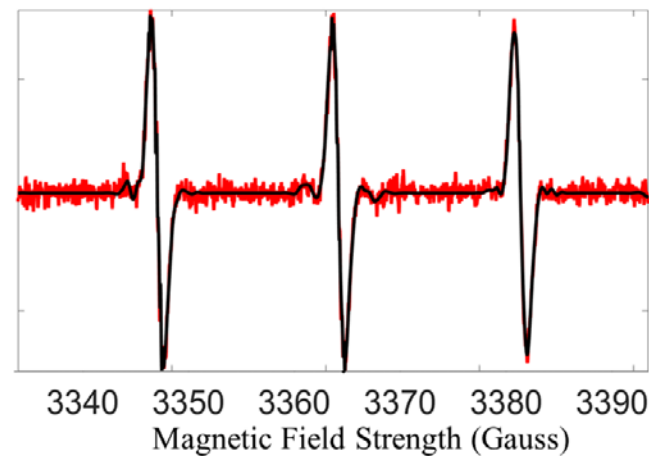
Signal	Noisy SNR	Denoised SNR
18 Scans	39	6×10^7
4 Scans	19	7×10^4
1 Scan	10	4×10^3

Sample: Tempol, 0.1mM in water at room temperature. X-Band 9.4GHz cw-ESR.

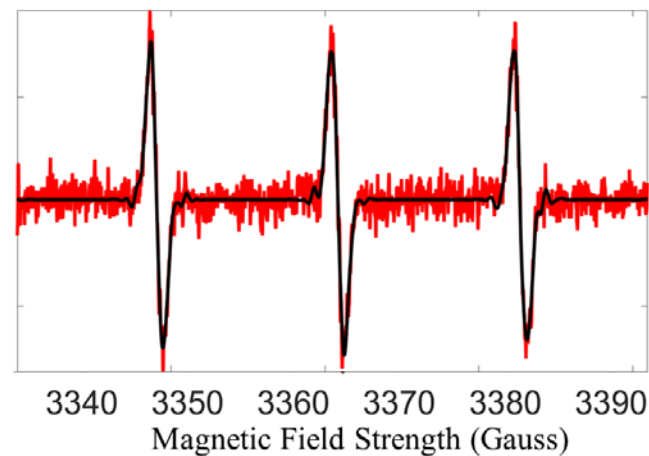
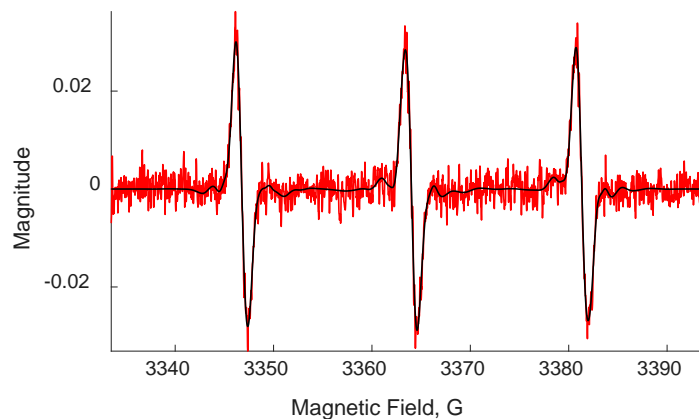
16 Scans Undecimated DWT



Decimated DWT



4 Scans



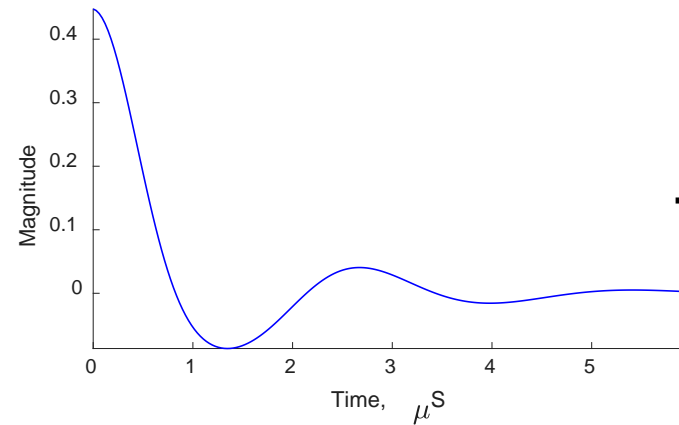
Signal		Noisy SNR	Denoised SNR
16 Scans	NERD	30	46416
	New Method	30	2220
4 Scans	NERD	14	2435
	New Method	14	784

Wavelet Denoising for Pulsed Dipolar Spectroscopy (WavPDS)

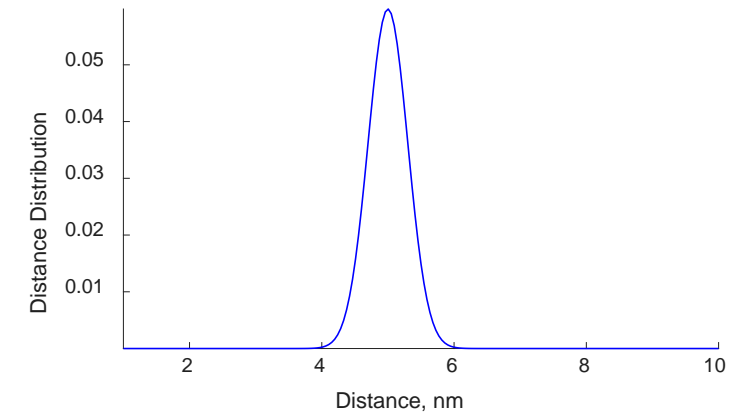
Sample



Dipolar Signal (S)



Distance Distribution (P)



Mathematical Formulation:

$$S(t) = \int_{R_{min}}^{R_{max}} K(r, t) P(r) dr$$

$S(t)$ - the experimental time-domain signal from spin pairs.

$P(r)$ - the distance distribution in pairs defined on the interval $[R_{min}, R_{max}]$.

$K(r, t)$ - the kernel for the Fredholm equation & can be of more complex form, if necessary.

Discrete Form:

$$KP = S$$

Matrix Inversion:

$$P = K^{-1}S$$



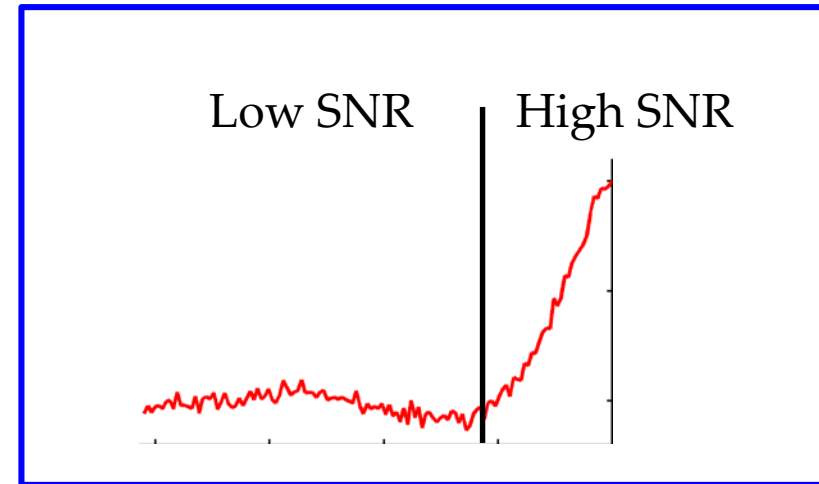
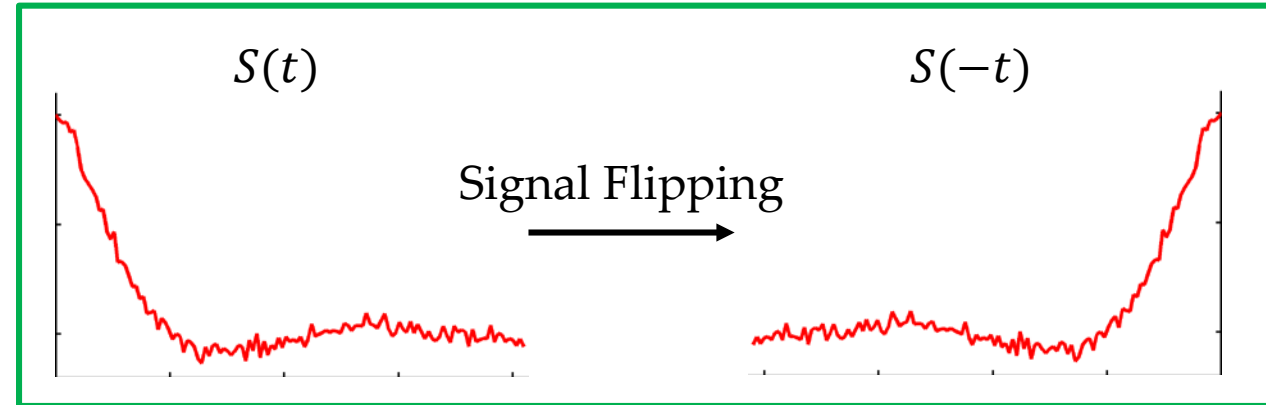
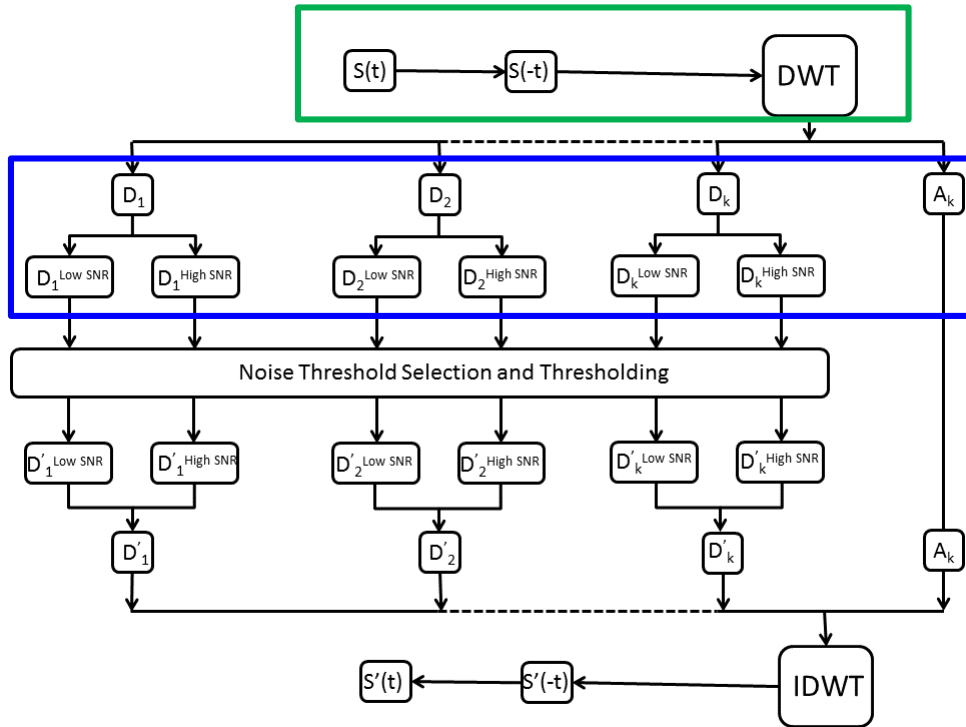
P cannot have single unique solution because K is singular, but see later.

Tikhonov Regularization:

$$\phi_{TIKR}[P] \equiv \min \|KP - S\|^2 + \lambda^2 \|LP\|^2$$

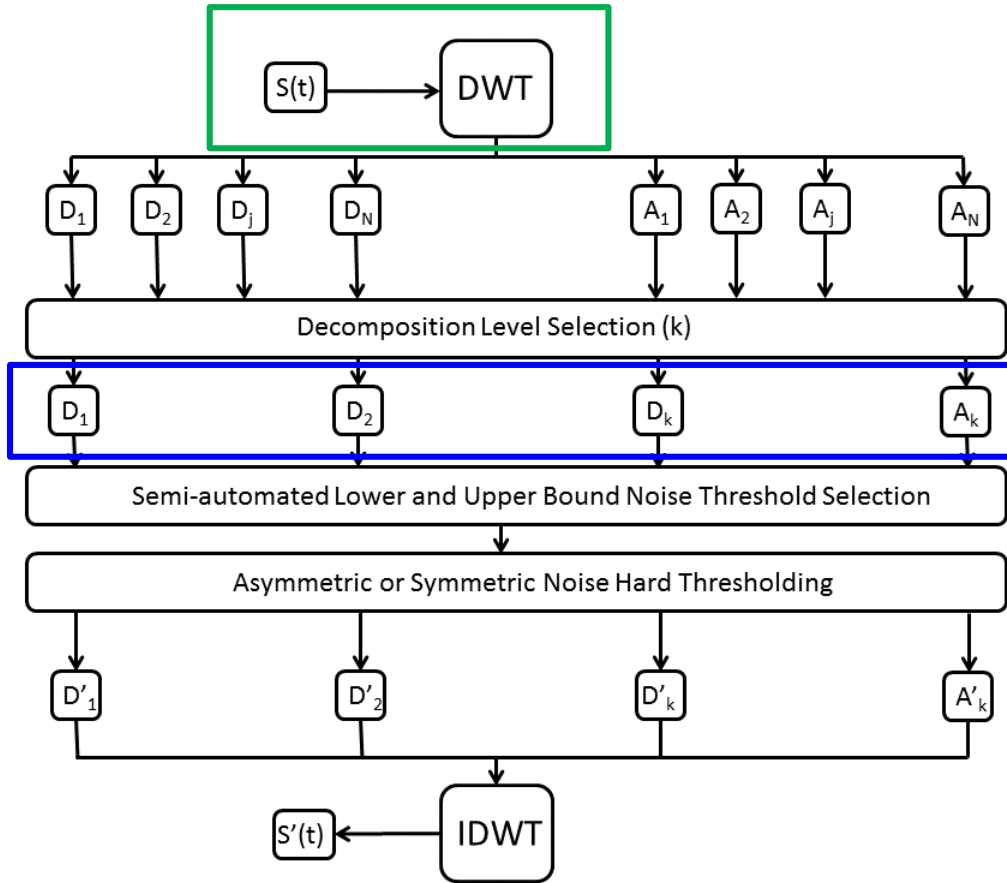
Regularization is used to obtain P

WavPDS

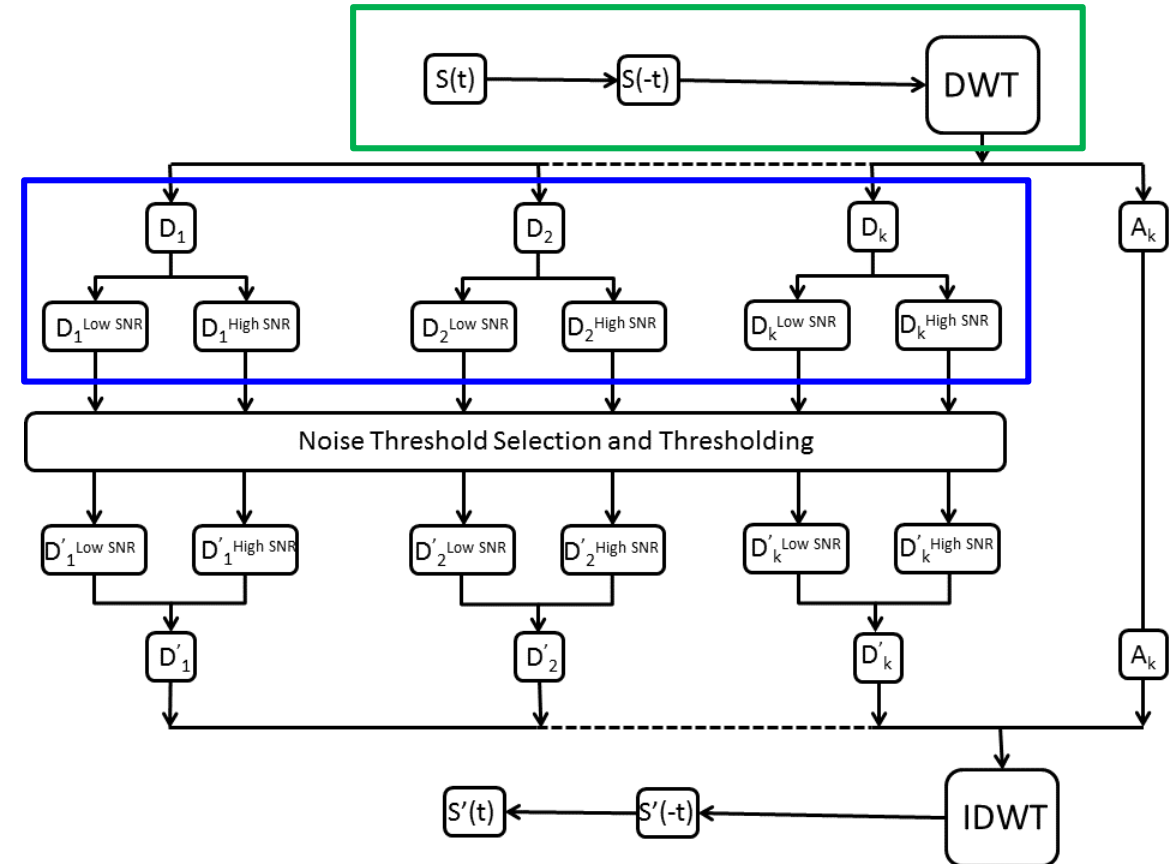


1. Flips the signal before applying DWT
2. Divides the signal into high and low SNR before noise thresholding

New Method (IEEE Paper):

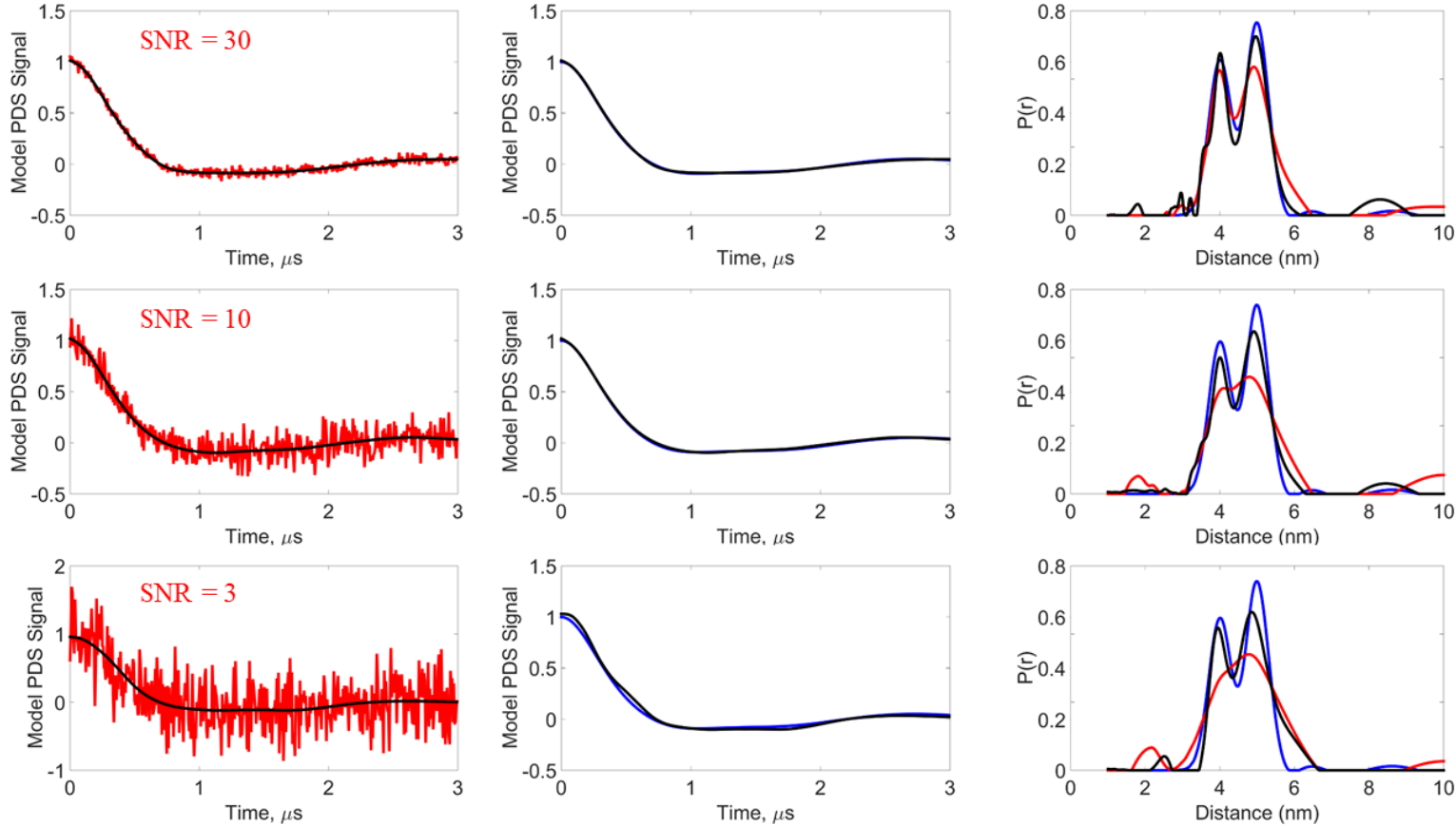


WavPDS



1. Flips the signal before applying DWT
2. Divides the signal into high and low SNR before noise thresholding

- Noisy
- Reference
- Denoised



	χ^2	SNR	SSIM
Noisy	4.3283	3	0.0077
	1.3999	10	0.1068
	0.4347	30	0.5412
Denoised	0.0363	378	0.7532
	0.0073	1850	0.9530
	0.0042	3186	0.9971

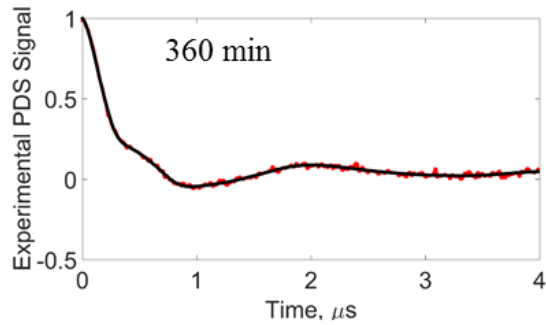
Model Data Generation: Two-Gaussians distance distribution with peaks at 4 and 5 nm were created, which was then converted to time-domain pulse dipolar signals.

Noise: Gaussian noise was added to create the signal with different SNRs.

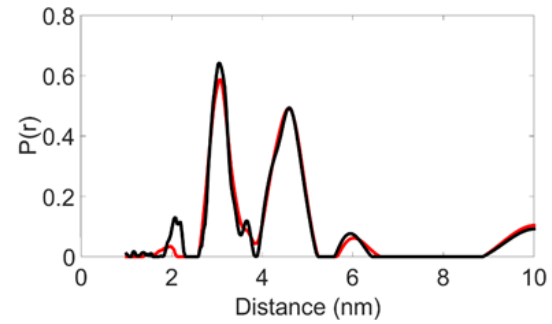
$$\chi^2 \equiv \sqrt{\frac{1}{p} \sum_{i=1}^p (f^{Ref}[i] - f[i])^2}$$

Wavelet: Daubechies 6

*Srivastava, Georgieva, Freed (2017) *J. Phys. Chem. A*



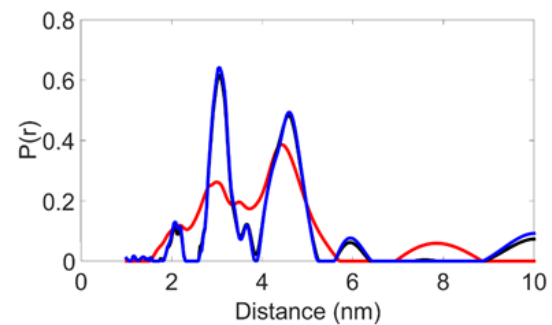
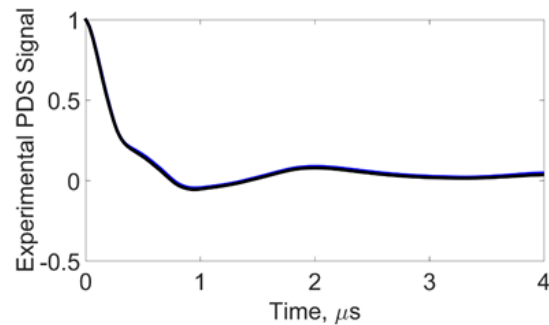
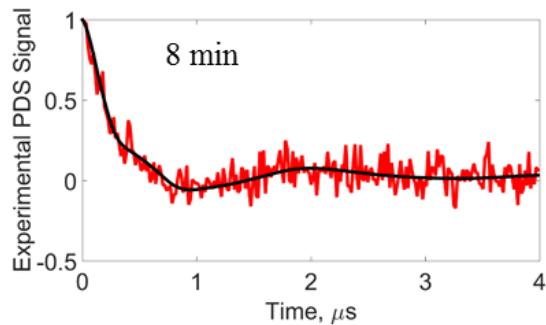
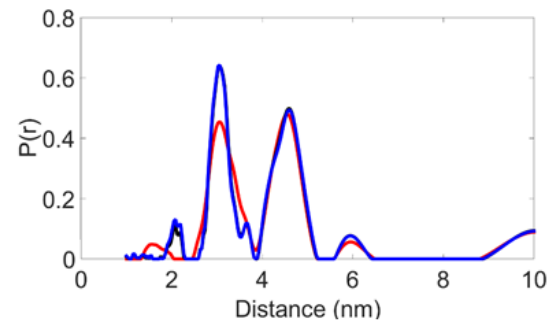
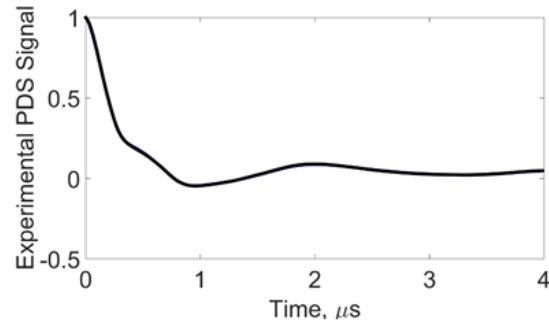
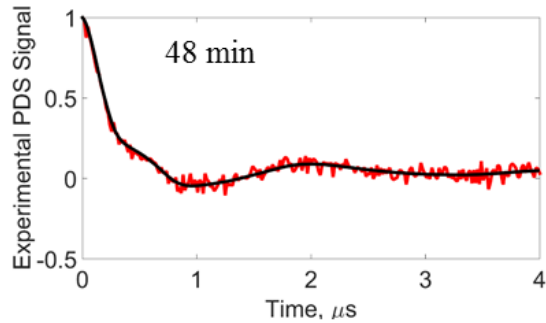
- **Noisy**
- **Reference**
- **Denoised**



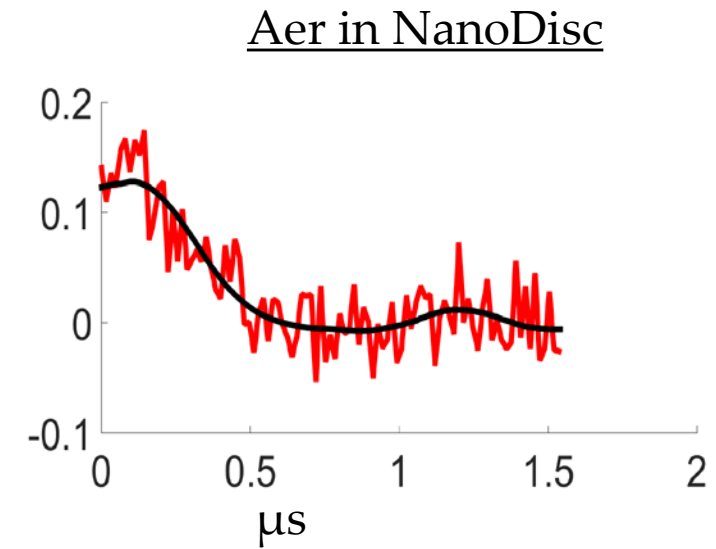
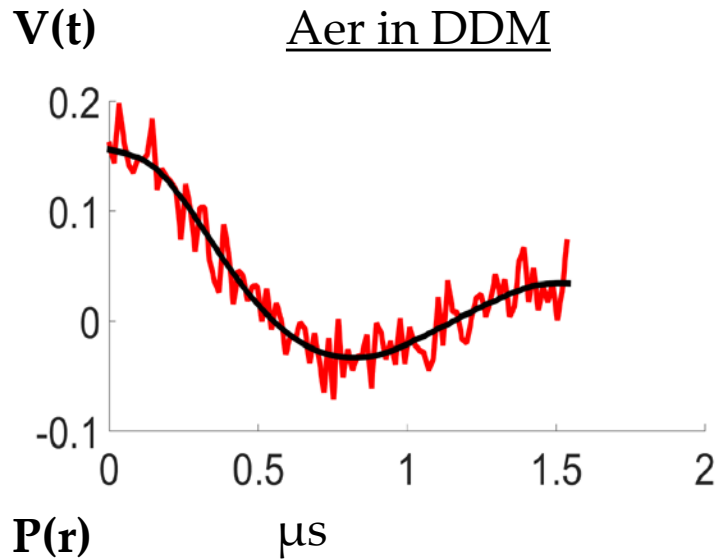
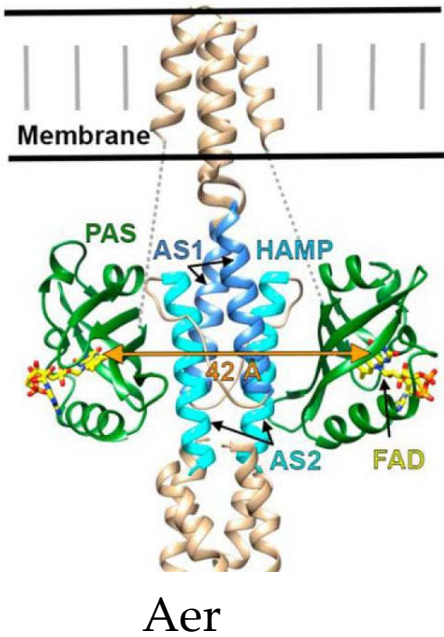
Wavelet: Daubechies 6

Sample:

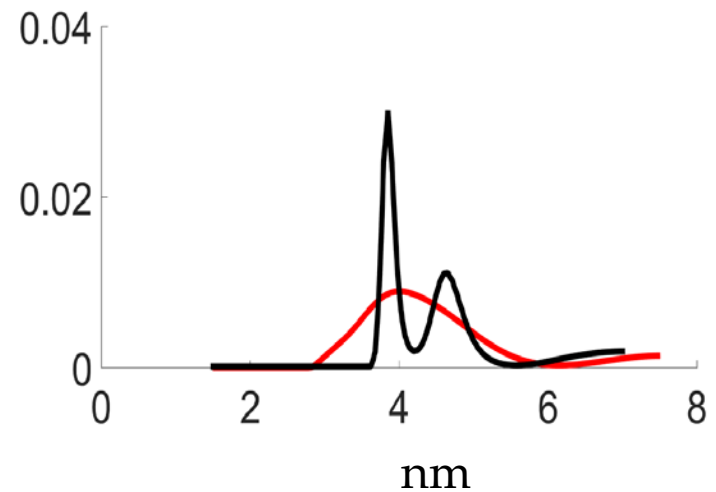
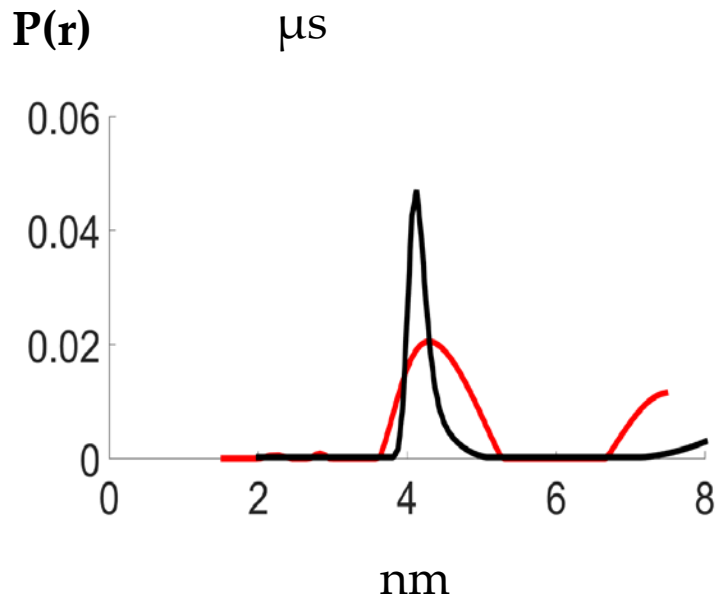
- Mut1/Mut2 MIX = 44 μ M/47 μ M.
- Mutants are T4 Lysozyme spin-labeled at H2O buff, 10% Gly + 20% Gly-d8



Signal Acquisition Time: 40 hrs



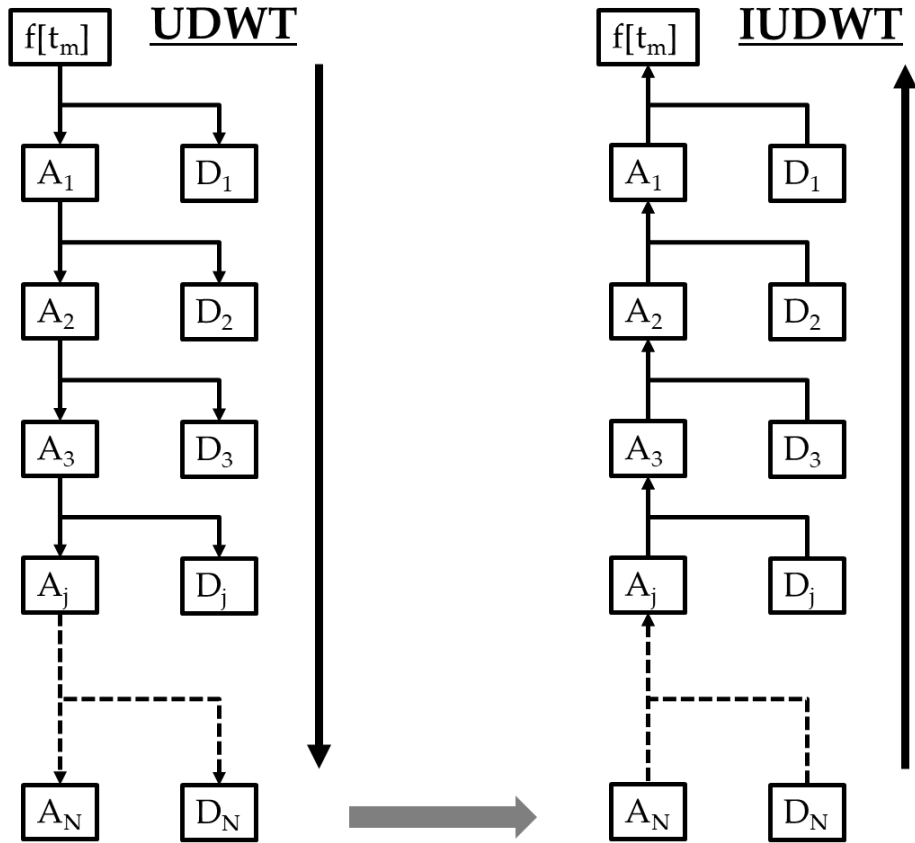
- Denoised
- Noisy



Sample:

- Flavin Adenine Dithionite spin-labeled Aer Solution = $60 \mu\text{M}$.
- Solution contains H₂O buff, 35% Gly

Undecimated DWT and IDWT



Approximation component

$$A_{j+1}[k] = \sum_{n=0}^{L-1} l[n] A_j[2k + n]$$

Detail component

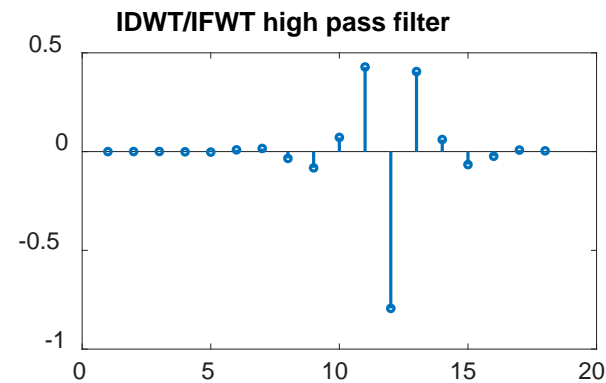
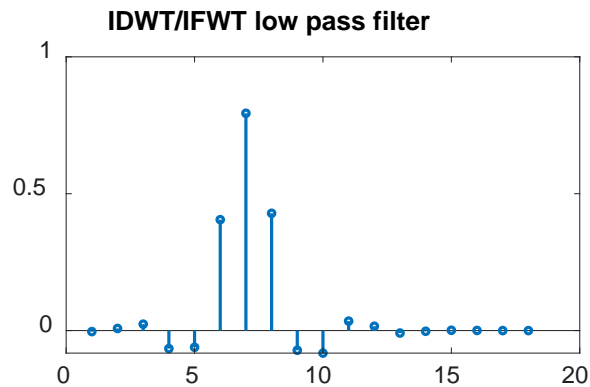
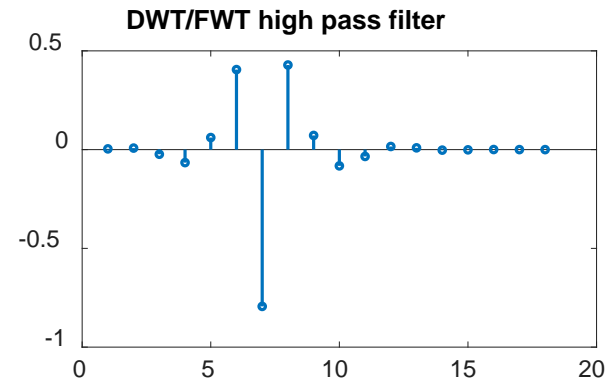
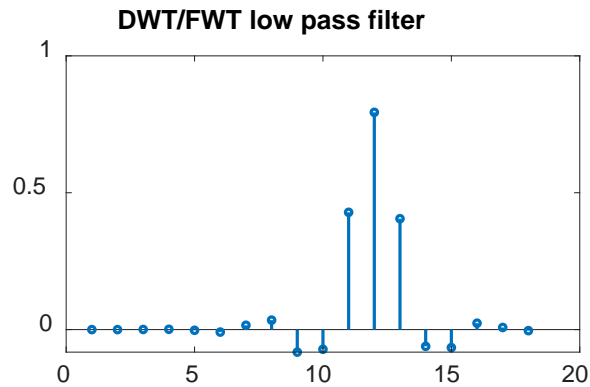
$$D_{j+1}[k] = \sum_{n=0}^{L-1} h[n] A_j[2k + n]$$

Inverse Fast Wavelet Transform

$$A_j[k] = \sum_{n=1}^{L-1} \tilde{l}[n] A_{j+1}[2k + n] + \sum_{n=1}^{L-1} \tilde{h}[n] D_{j+1}[2k + n]$$

$l[n]$ and $\tilde{l}[n]$ = low pass filters
 $h[n]$ and $\tilde{h}[n]$ = high pass filters

Coiflet 3



FWT: Relation between low and high pass filters

$$h[n] = (-1)^n l[L - 1 - n]$$

IFWT: Relation between low and high pass filters

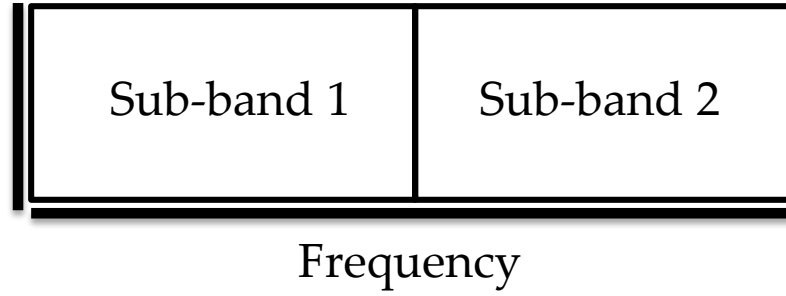
$$\tilde{h}[n] = (-1)^n \tilde{l}[L - 1 - n]$$

Relation between FWT and IFWT filters

$$\tilde{h}[n] = h[L - 1 - n]$$

$$\tilde{l}[n] = l[L - 1 - n]$$

a Non-overlapping Frequency Sub-band



b Overlapping Frequency Sub-band

